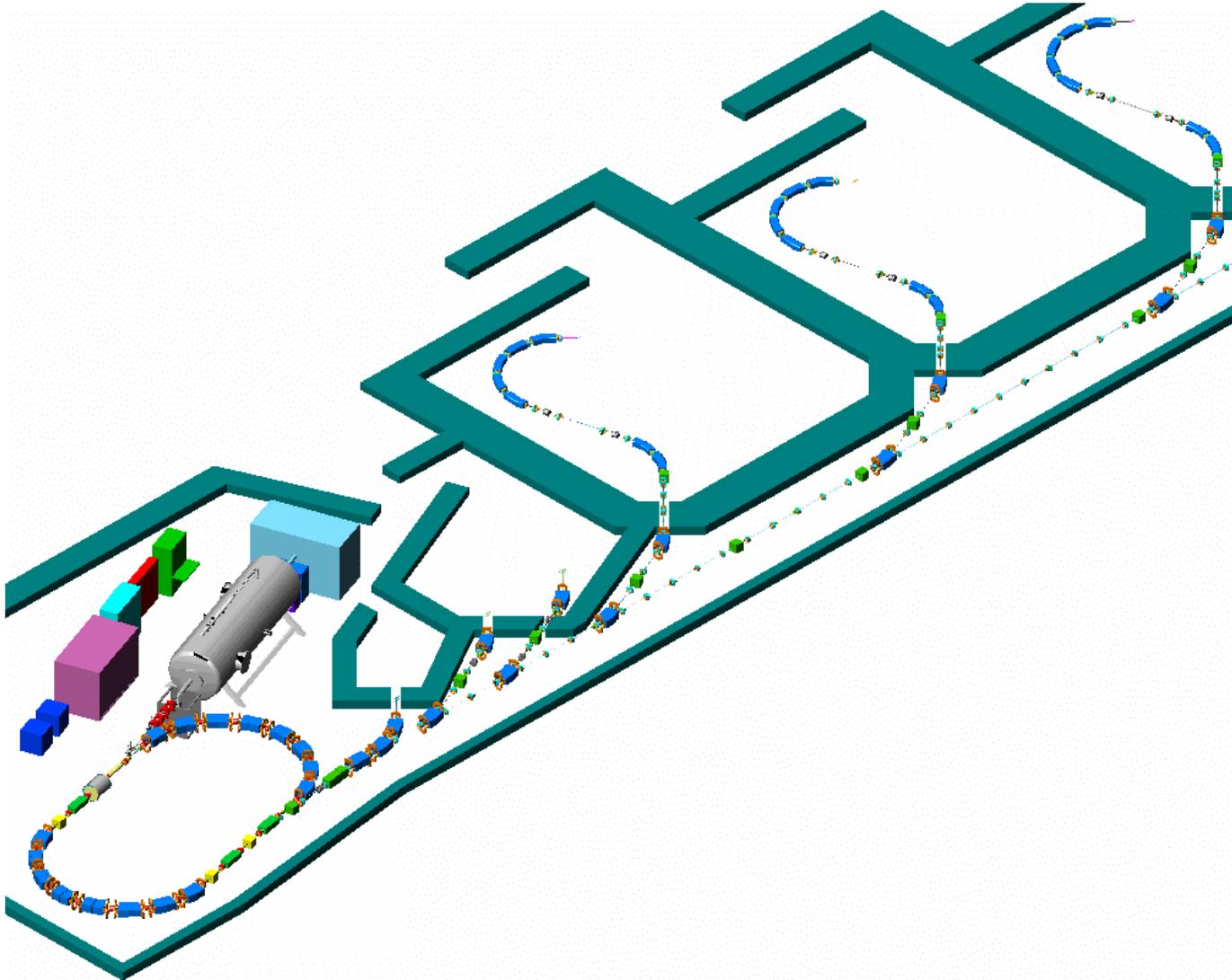


# Proton Therapy & Proton Imaging

Steve Peggs, BNL



# Contents

## Proton Therapy

**Why protons? Why now? Where?**

**Precision 3-D multi-field irradiation of cancerous tumors**

## Proton Imaging

**Proton driven PET**

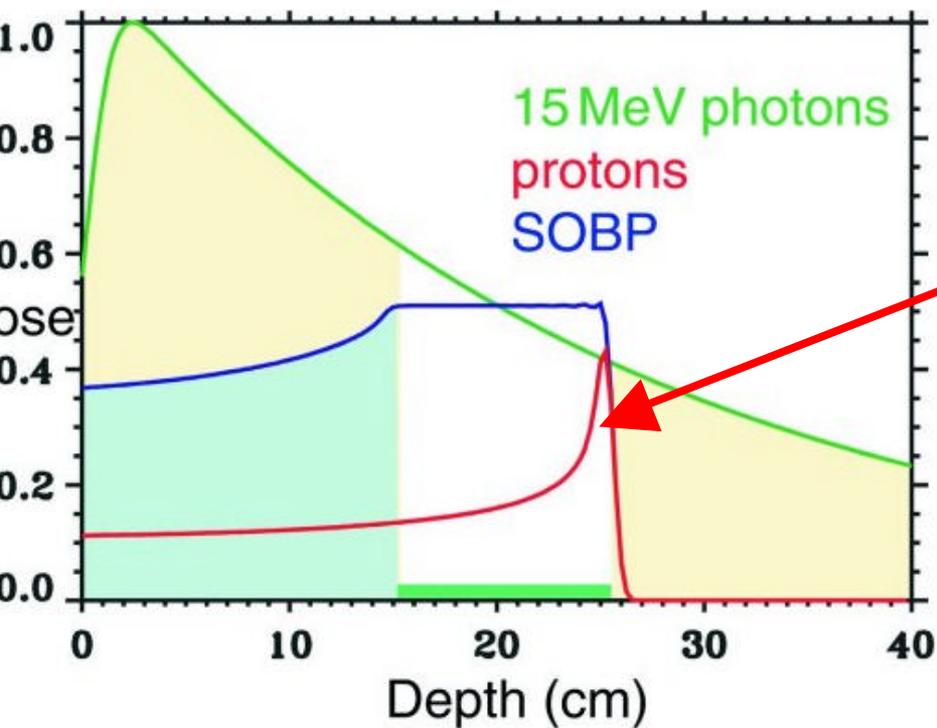
**Proton CT**

**Transient devices: PRAD movies**

**Periodic CT = pCT + PRAD ??**

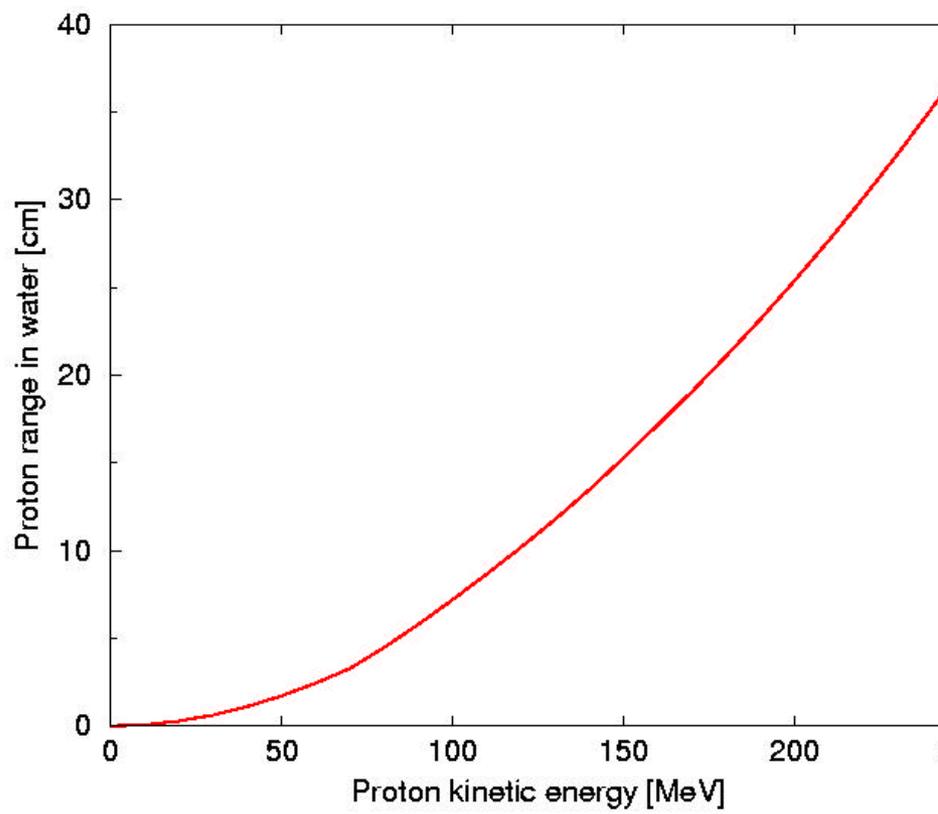
**Why protons? Why now? Where?**

# Protons are much better than X-rays



Most dose is deposited in the sharp "Bragg Peak", with no dose beyond

Scan the energy to make a Spread Out Bragg Peak (SOBP) that spans the tumor



# Conventional X-Ray gantries are small

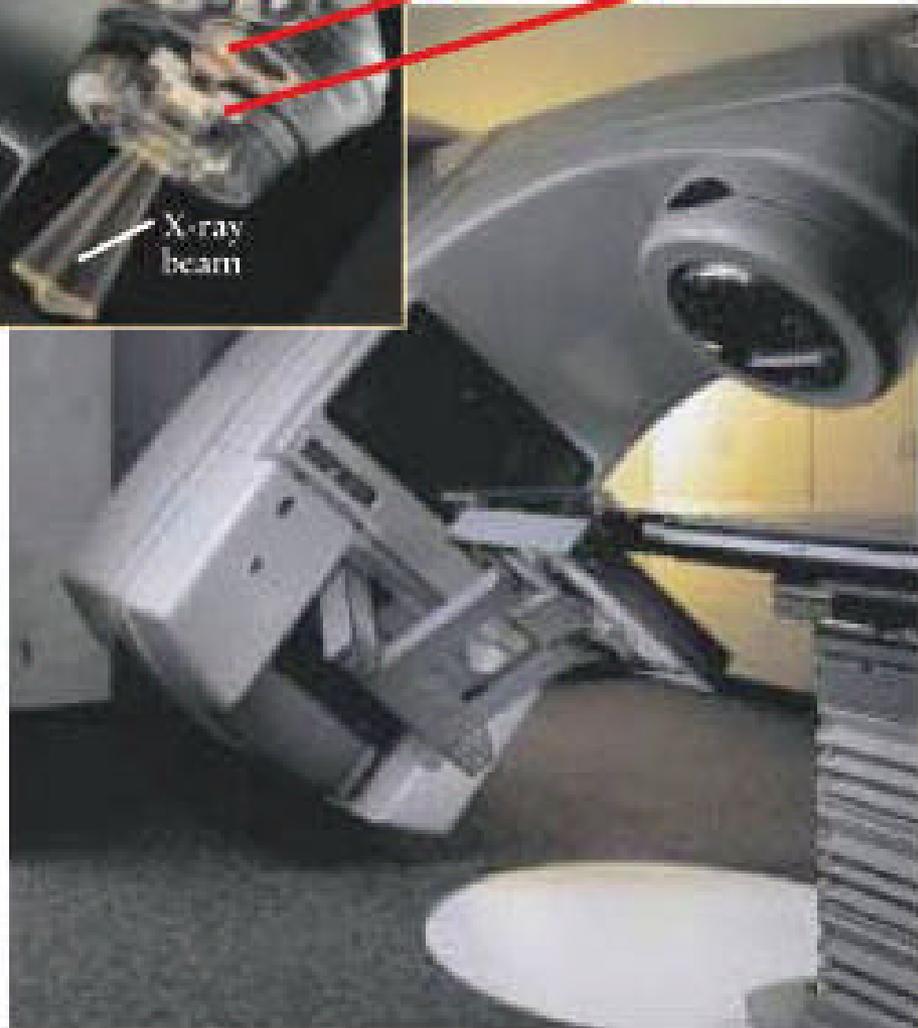
linear accelerator

Bending Magnet

Targets on retractable piston

Flattening filters on turret

Collimators

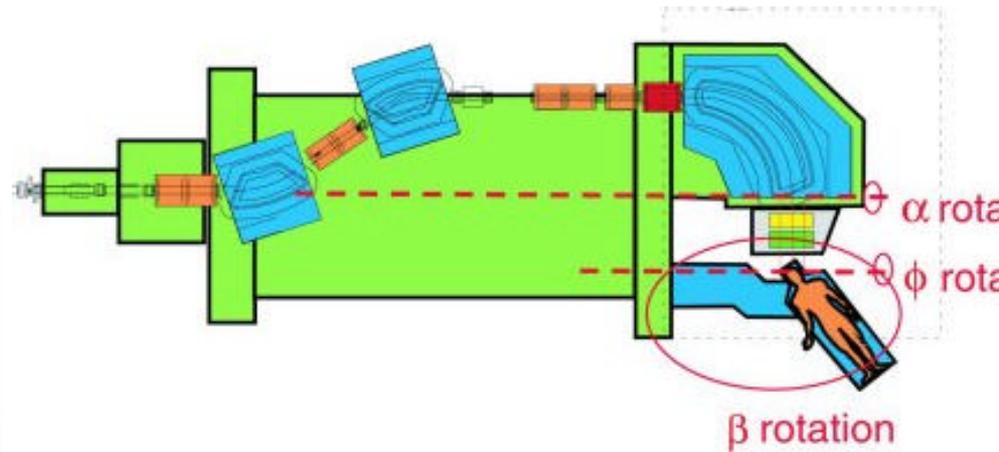


**Almost all of it is visible in this photograph!**

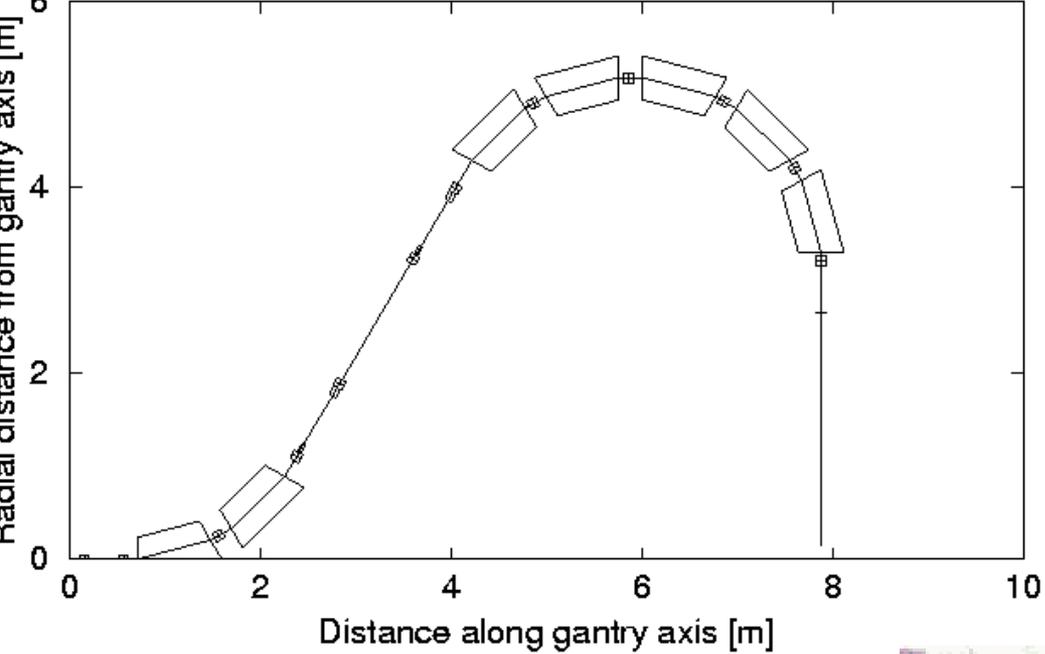
# Proton gantries appear similar to the patient



But there is a lot more  
"behind the wall"



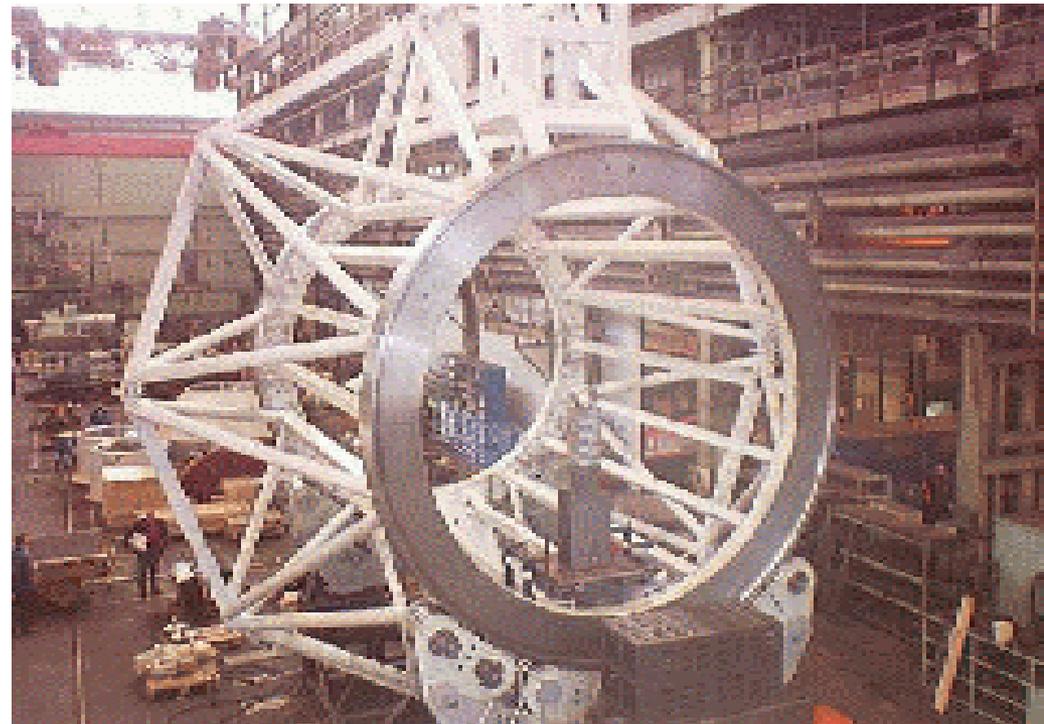
Paul Scherrer Institute (PSI), Zurich

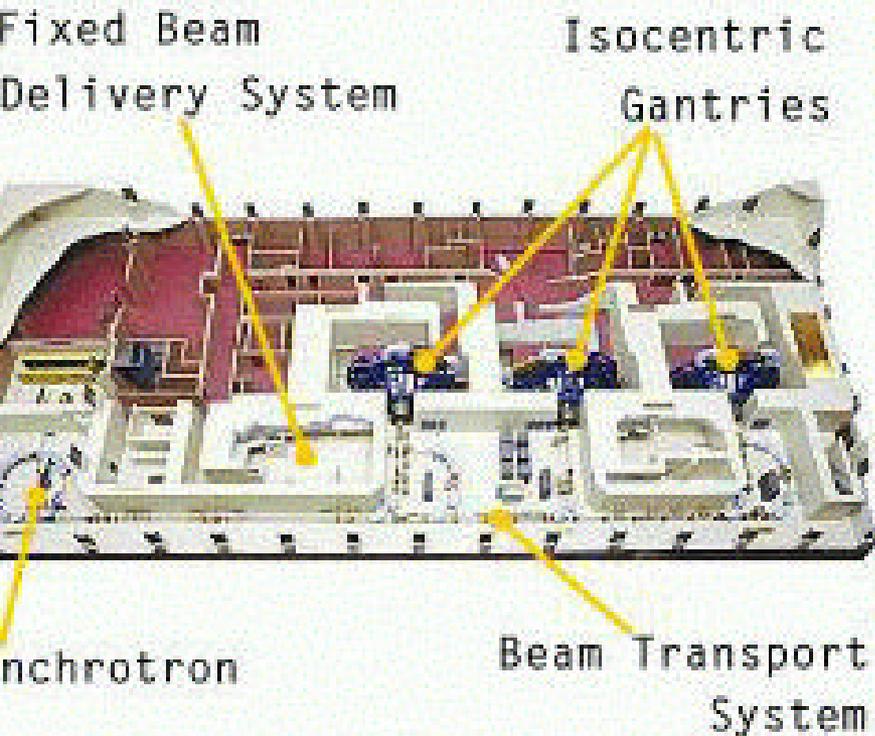


**It's much harder to bend 250 MeV protons**

**And the strong-back to hold 1 mm tolerances is formidable**

Massachusetts General Hospital (MGH)



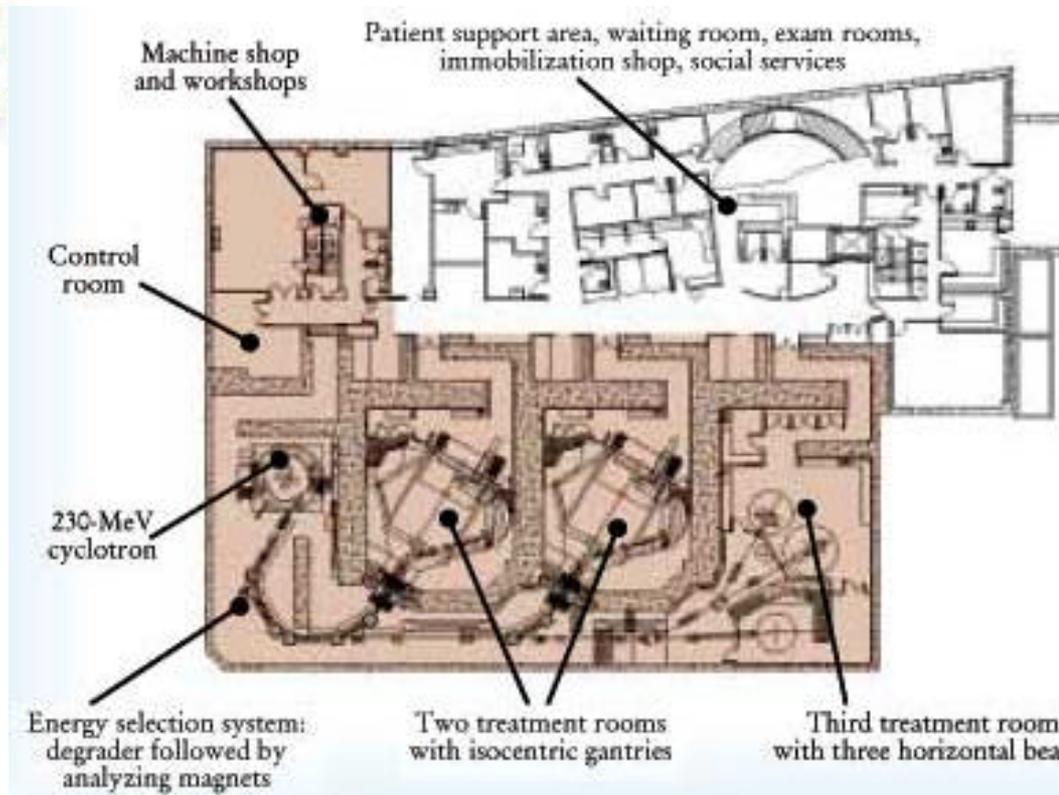


## Loma Linda (California)

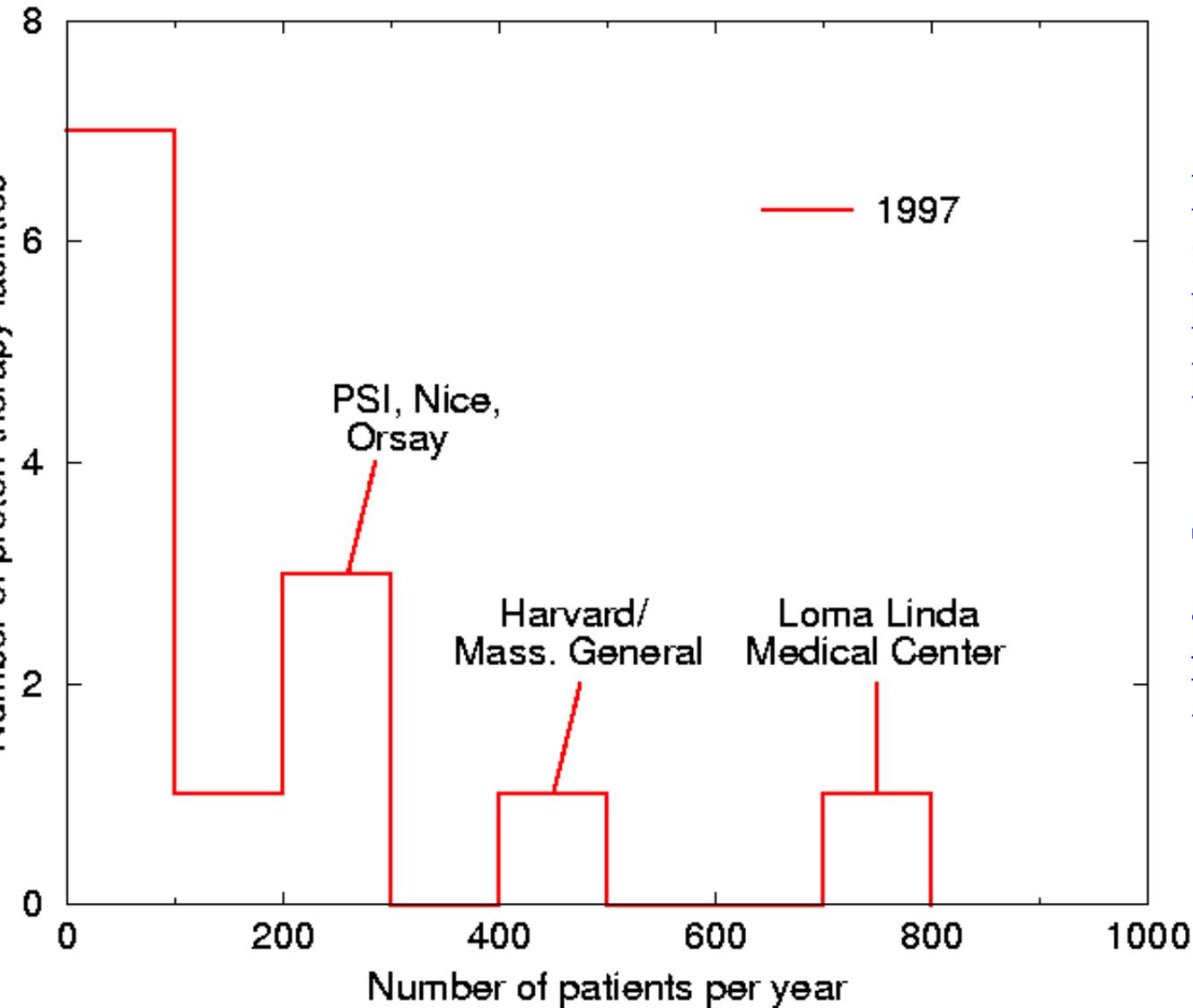
- **synchrotron source**
- **built/commissioned at Fermilab**
- **world leading patient throughput**

## MGH (Boston)

- **cyclotron source (IBA)**
- **1<sup>st</sup> patient Nov 2001**
- **coming up to speed**

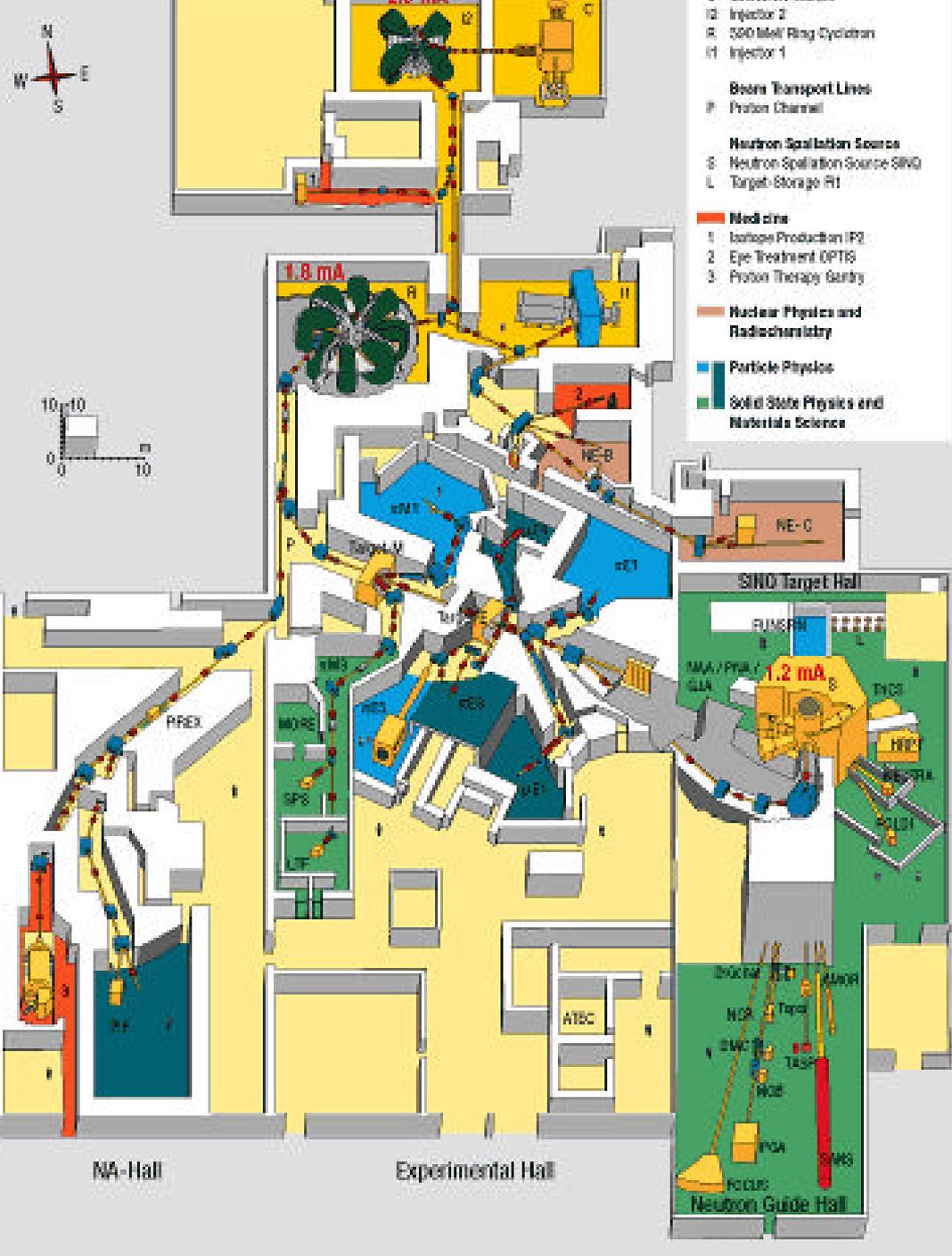


# High and low patient throughput



Loma Linda and MGH  
(hospital based facilities)  
lead the world in **high**  
patient throughput

The state-of-the-art is  
also being pushed in  
facilities at national labs  
with **low** throughput



## PSI (Zurich) (left)

- cyclotron source
- part of a national lab
- upgrade in progress
- low throughput, high tech
- new facility in progress

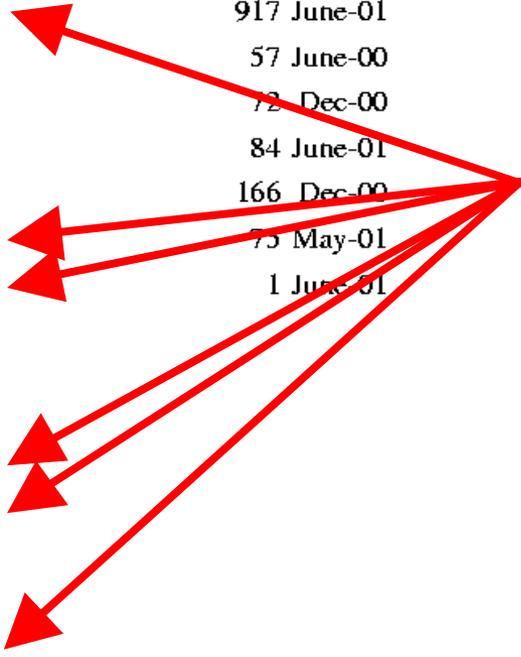
## GSI (Darmstadt) (not shown)

- synchrotron
- national lab
- Carbon-12
- new facility at Heidelberg?

			Date	Patient Total
Moscow	Russia	p	1969	3414 June-01
St. Petersburg	Russia	p	1975	1029 June-98
Chiba	Japan	p	1979	133 Apr-00
PSI (72 MeV)	Switzerland	p	1984	3360 July-00
Dubna	Russia	p	1987	88 May-01
Uppsala	Sweden	p	1989	236 June-00
Clatterbridge	England	p	1989	1033 Dec-00
Loma Linda, Cal.	USA	p	1990	6174 June-01
Nice	France	p	1991	1590 June-00
Orsay	France	p	1991	1894 Jan-01
N.A.C.	South Africa	p	1993	398 June-01
MPRI, Indiana	USA	p	1993	34 Dec-99
UCSF - CNL, Cal.	USA	p	1994	284 June-00
HIMAC, Chiba	Japan	ion	1994	917 June-01
TRIUMF	Canada	p	1995	57 June-00
PSI (200 MeV)	Switzerland	p	1996	72 Dec-00
GSI Darmstadt	Germany	ion	1997	84 June-01
Berlin	Germany	p	1998	166 Dec-00
NCC, Kashiwa	Japan	p	1998	75 May-01
HARIMAC, Hyogo	Japan	p, (ion)	2001	1 June-01
INFN-LNS, Catania	Italy	p	2001	
NPTC - MGH, Mass.	USA	p	2001	
NAC, Faure	South Africa	p	2001	
Tsukuba	Japan	p	2001	
Wakasa Bay	Japan		2002	
Bratislava	Slovakia	p, ion	2003	
IMP, Lanzhou	China	C-Ar ion	2003	
Shizuoka	Japan		2003	
Rinecker, Munich	Germany	p	2003	

**The last decade has seen much construction activity**

**There is a national program in Japan to build proton (and Carbon-12) facilities**

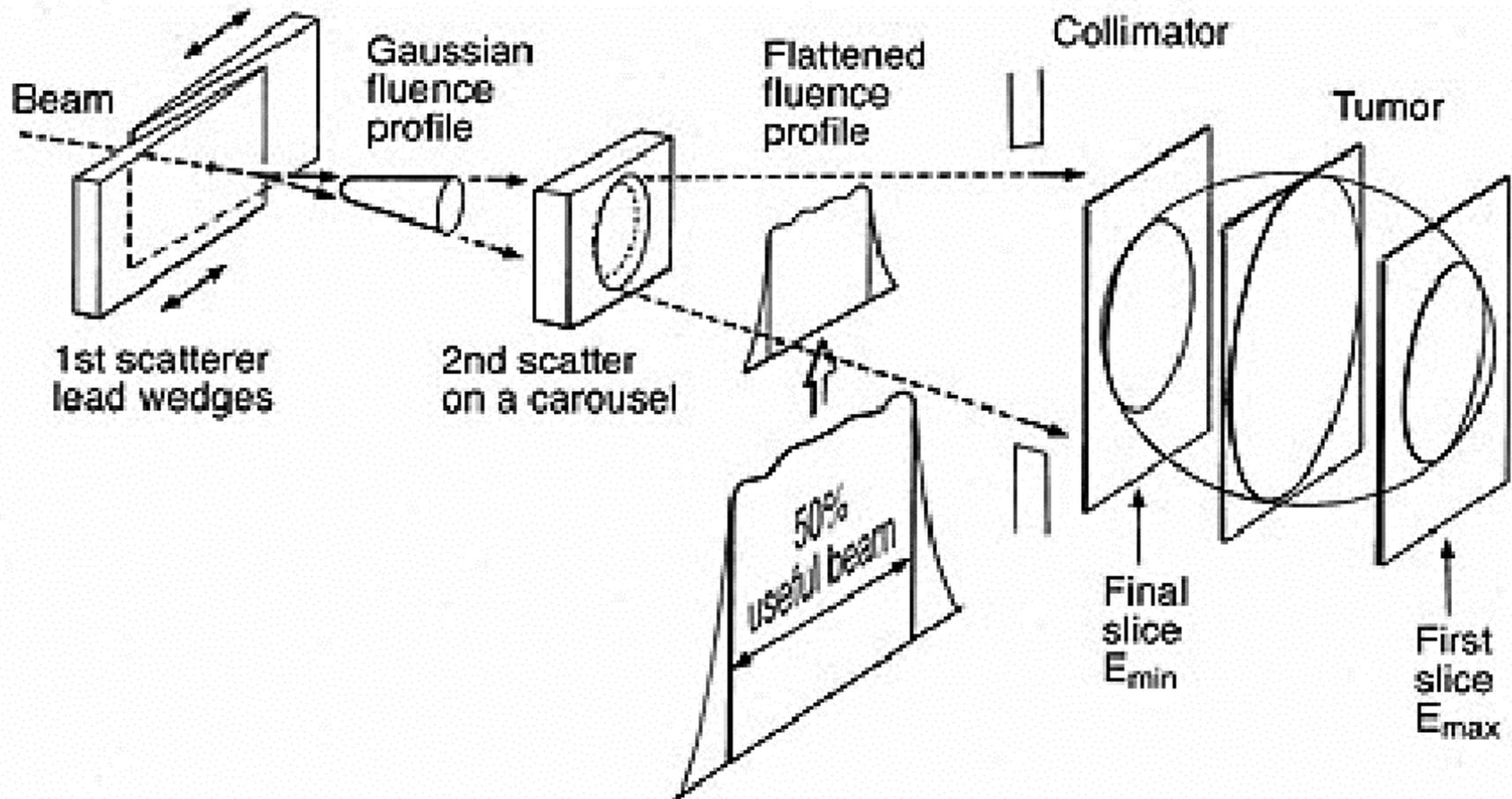


**The continuous upgrade path**

to

**precision 3-D multi-field irradiation  
of cancerous tumors**

# Traditional irradiation: PASSIVE SCATTERING



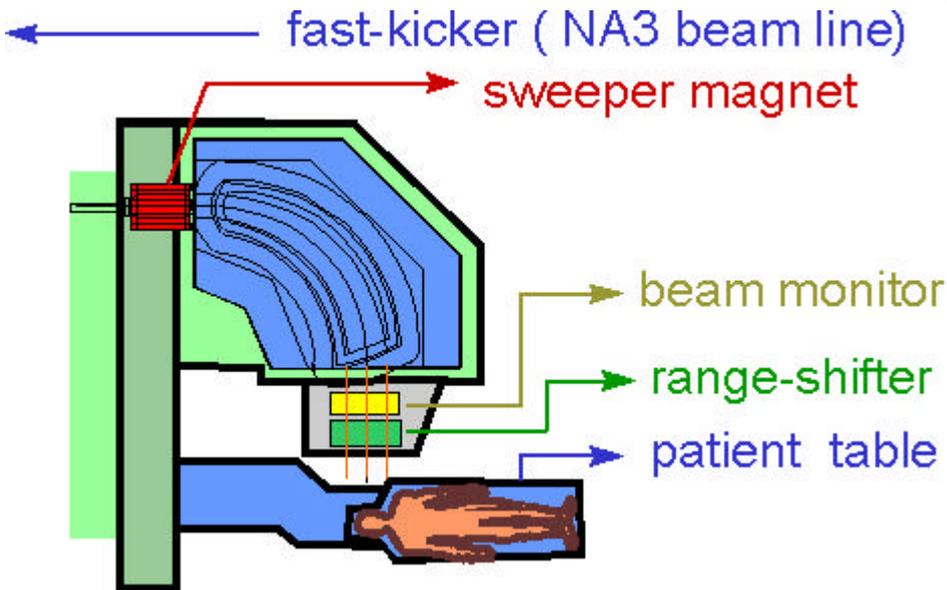
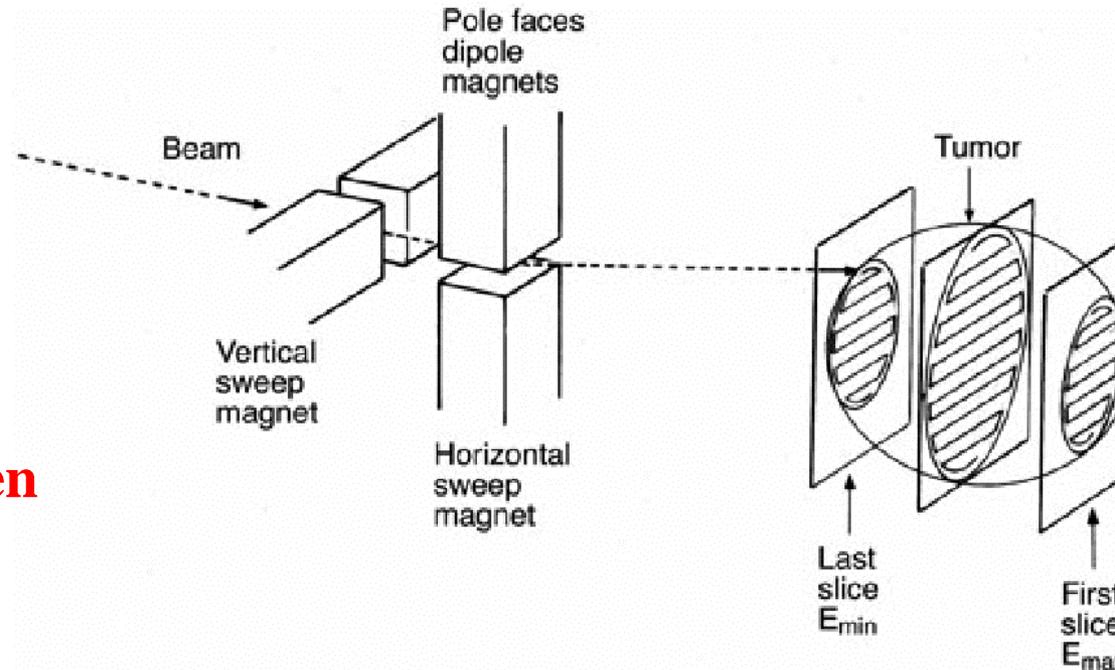
The sole (slow) variation: beam energy  $\rightarrow$  depth

# Contemporary Irradiation: ACTIVE SCANNING

Three variables:

- H & V steering
- energy

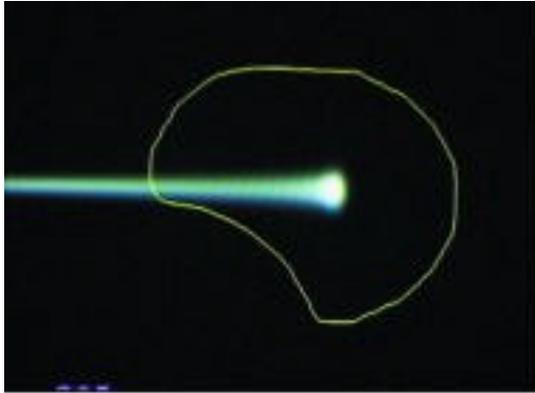
Although "simpler",  
active scanning has a  
higher controls burden



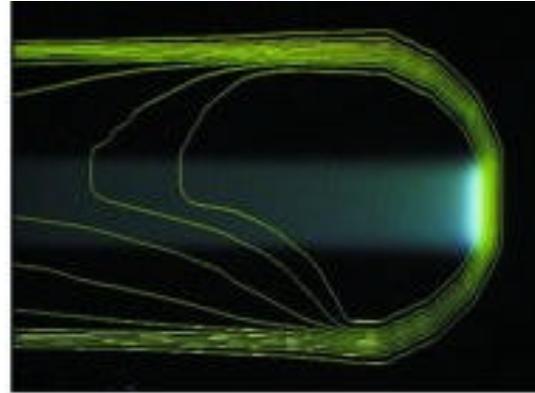
Hybrid schemes are also  
practical (PSI, left)

- 1.5 D steering
- range shifter

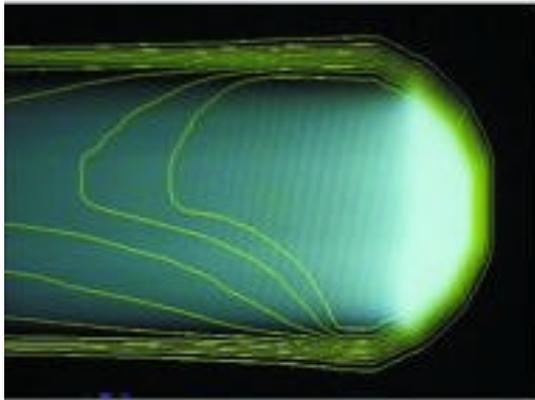
# Active scanning - a much improved 3-D conformal dose



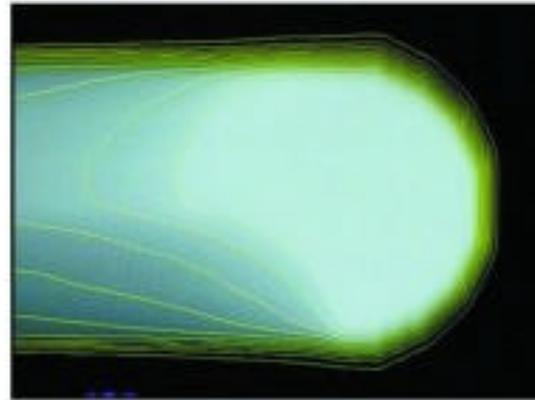
Single beam...



( lateral scanning



+ scanning in depth

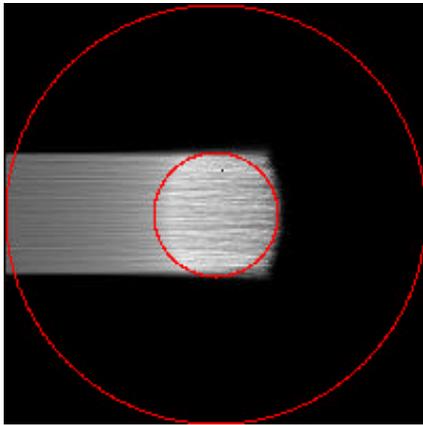


= 3d conformed dose)

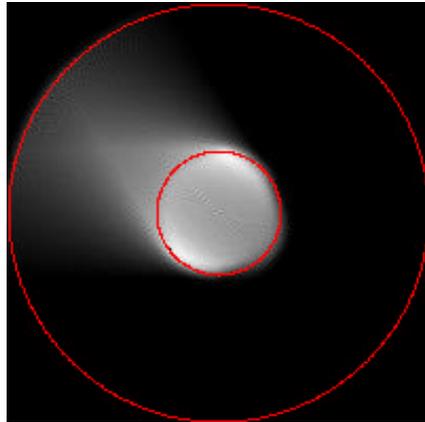
**(Patient treatment demos courtesy of PSI)**

# Multiple angles with a water phantom

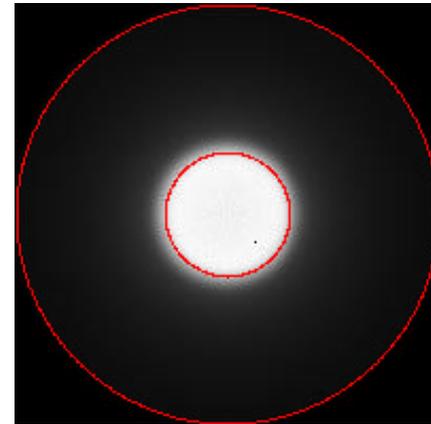
One angle



60 degree coverage

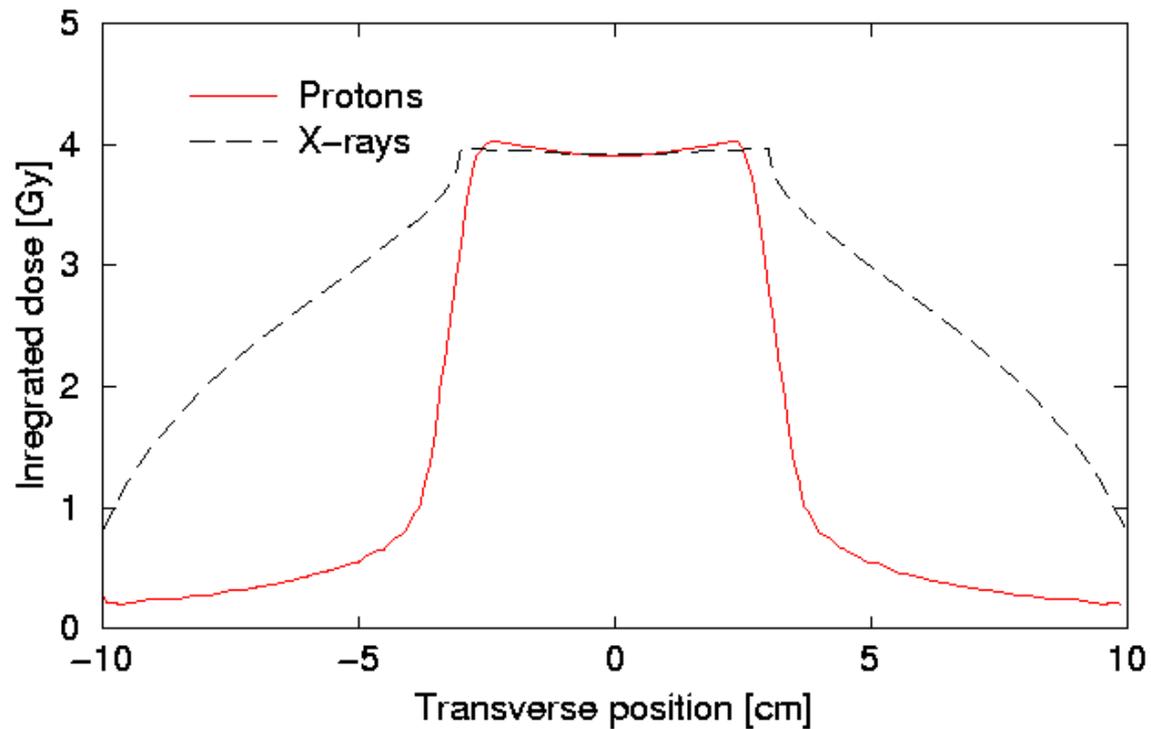


360 degrees



Ultra-low level collateral radiation with protons ...

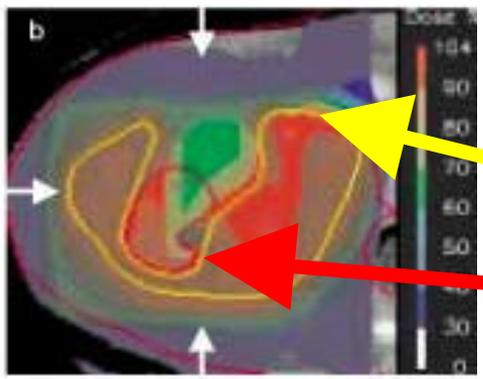
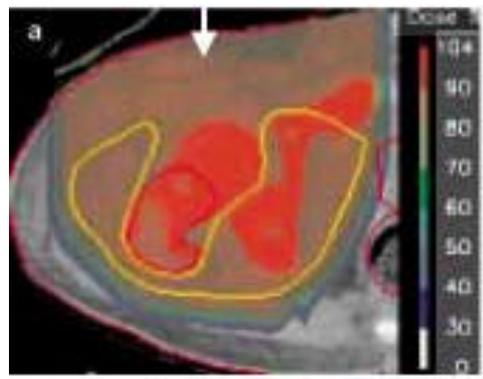
... if ultimate multi-dimensional flexibility can be achieved !



1 field, passive scattering

3 fields, passive

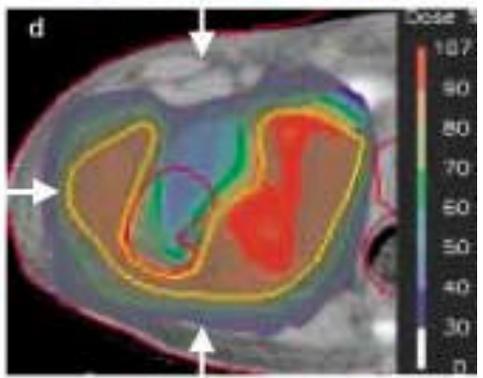
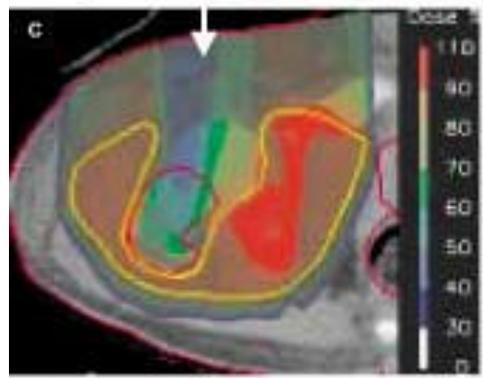
POOR



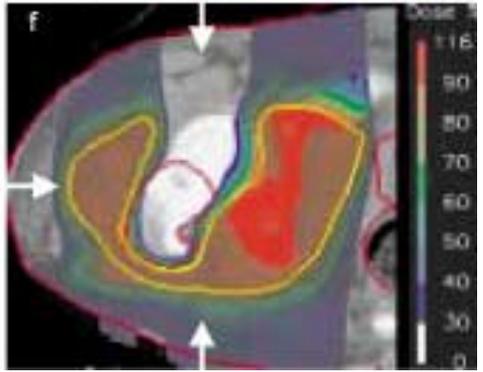
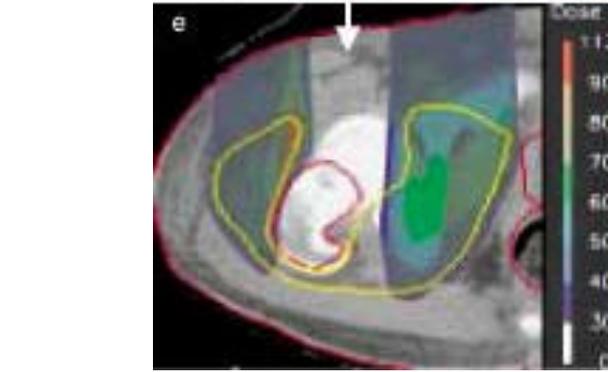
Target outlined in yellow

Critical structures in red

1 field, active, uniform dose



3 fields, active, uniform dose



GOOD

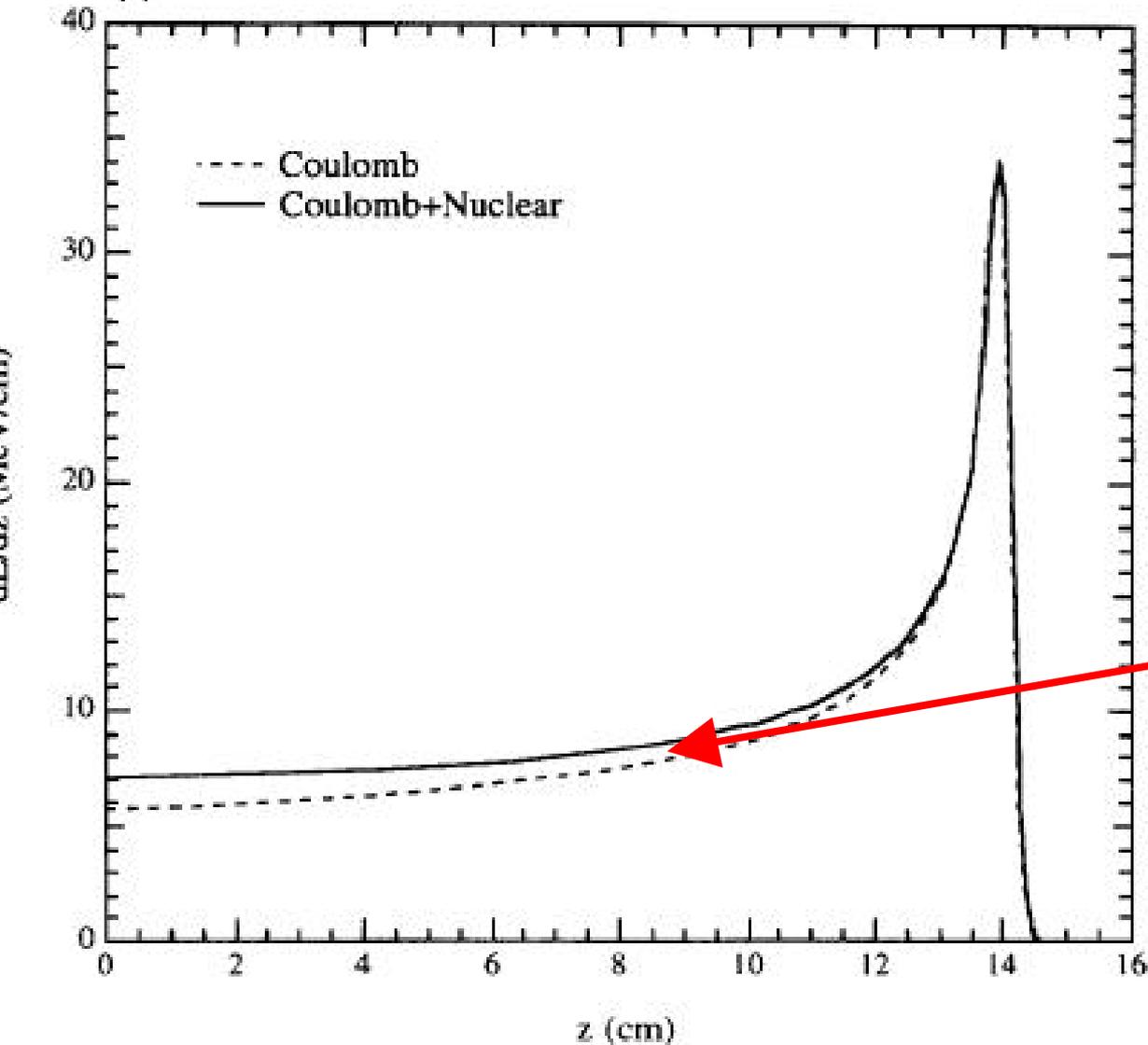
Bottom right is much better than top left!

1 field of 3, active, intensity modulated

3 of 3 fields, active, intensity modulated

# Proton Driven PET

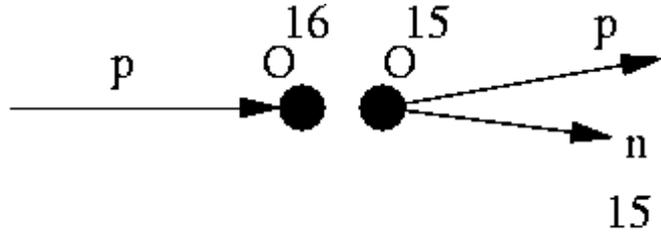
# Nuclear cross sections matter, and are useful!



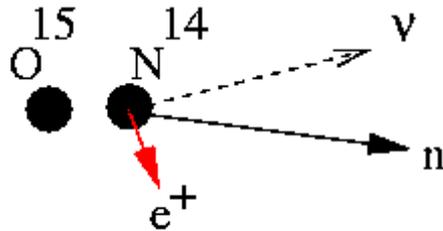
A small but significant fraction of proton  $dE/dx$  loss is due to nuclear interactions

some of which generate positron emitters

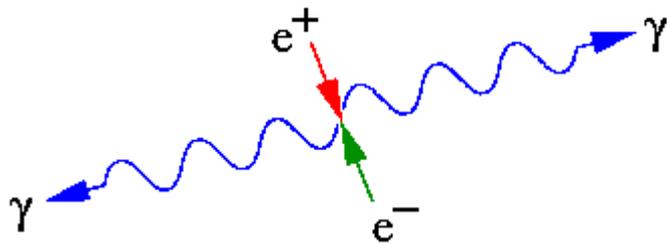
# Is the (high) therapy dose going to the right place?



Occasionally a proton generates an  $O^{15}$  isotope ...



... that decays by emitting a positron ...



... which annihilates with an electron

**Place a PET camera on the gantry to observe where such nuclear interactions occur**

**Nuclear cross sections vary rapidly with energy ...**

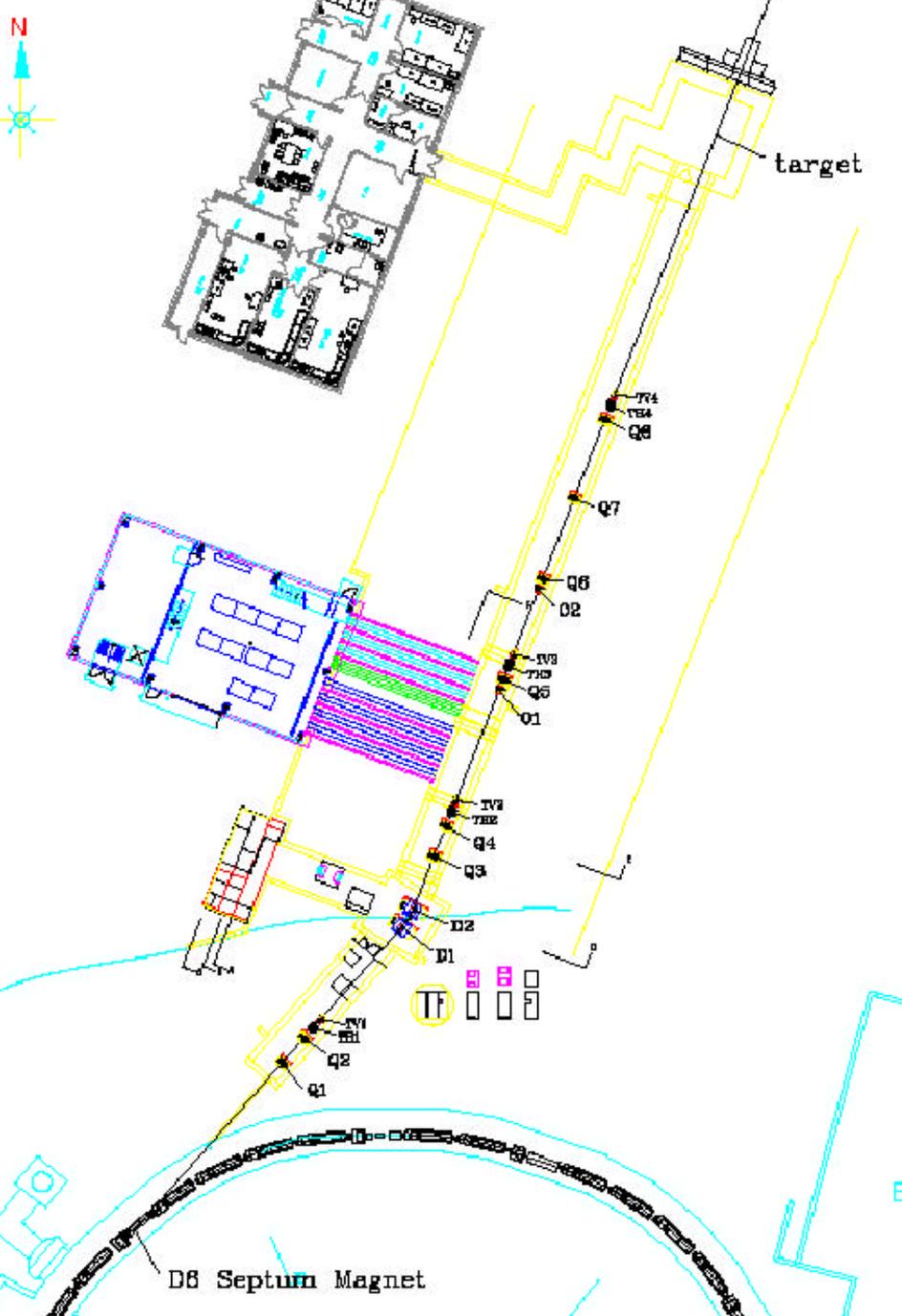
**Interesting work is also going on with C-12 driven PET, eg at GSI (Parodi et al)**



**Include a PET camera like this (at BNL) in a gantry room for best possible co-registration of tumor and beam**

**Preliminary studies are under way at PSI (also with Carbon-12) and at BNL**

# **Proton Computed Tomography - pCT**



**The "pCT" collaboration  
is forming (?)**

- BNL
- Loma Linda
- UC Santa Cruz
- Stony Brook

**First meeting/workshop -  
Thurs/Fri Jan 9 & 10**

**The BAF beamline appears  
to be an ideal location for  
pCT R&D !**



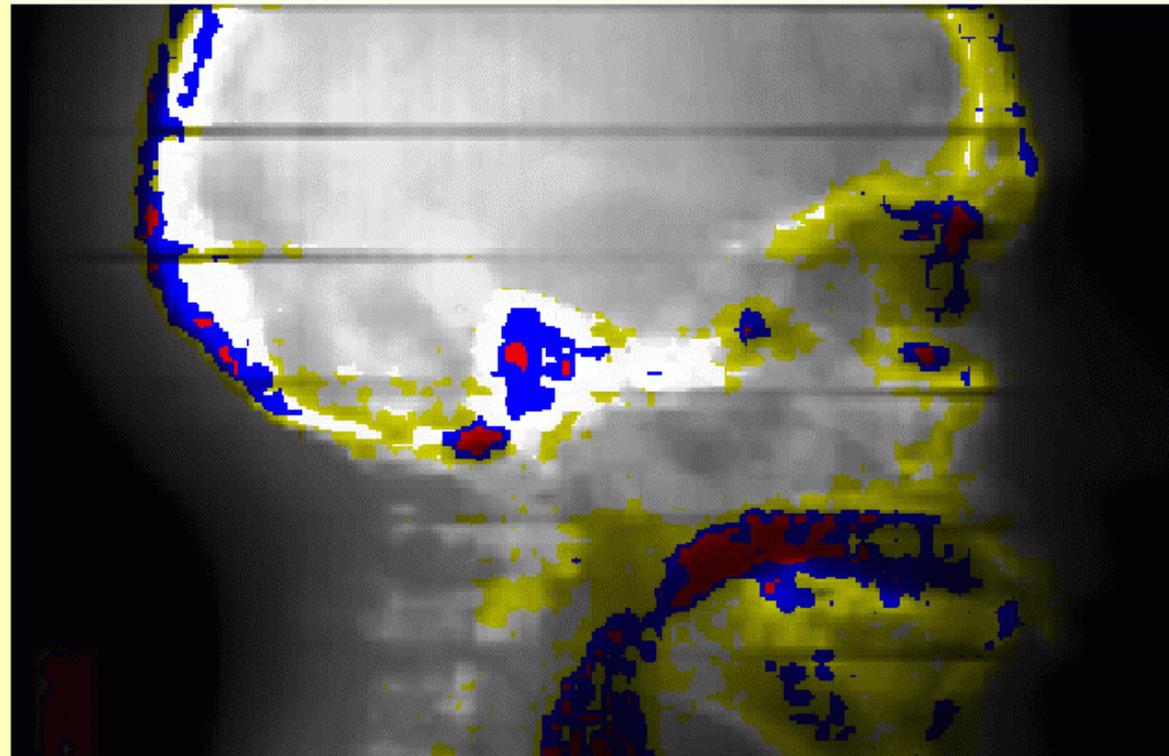
# Use of Proton Beam CT: Treatment Planning

X-ray CT use in Proton Cancer Therapy can lead to large Uncertainties in Range Determination

## Range Uncertainties (measured with PTR)

-  > 5 mm
-  > 10 mm
-  > 15 mm

Schneider U. & Pedroni E. (1995),  
"Proton radiography as a tool for  
quality control in proton therapy," Med  
Phys. 22, 353.

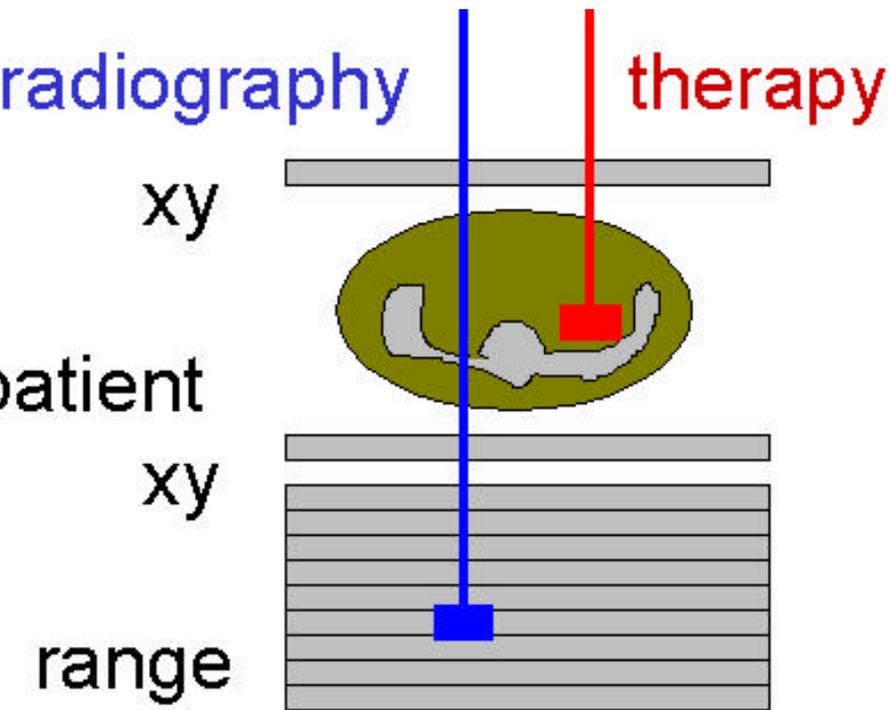


**Alderson Head Phantom**

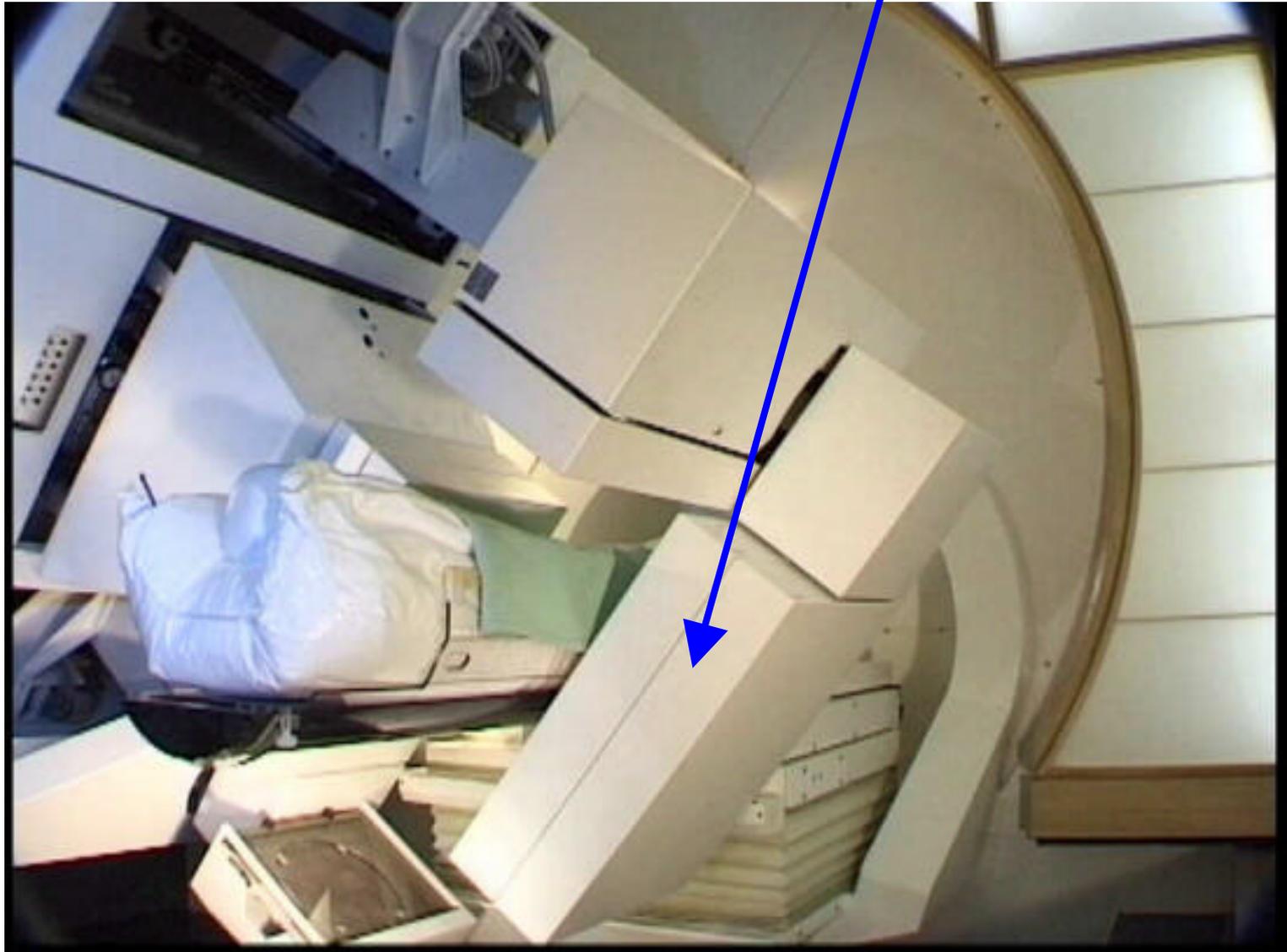
# Prototype detector at PSI

The protons go through the patient  
Higher energy, **small dose**

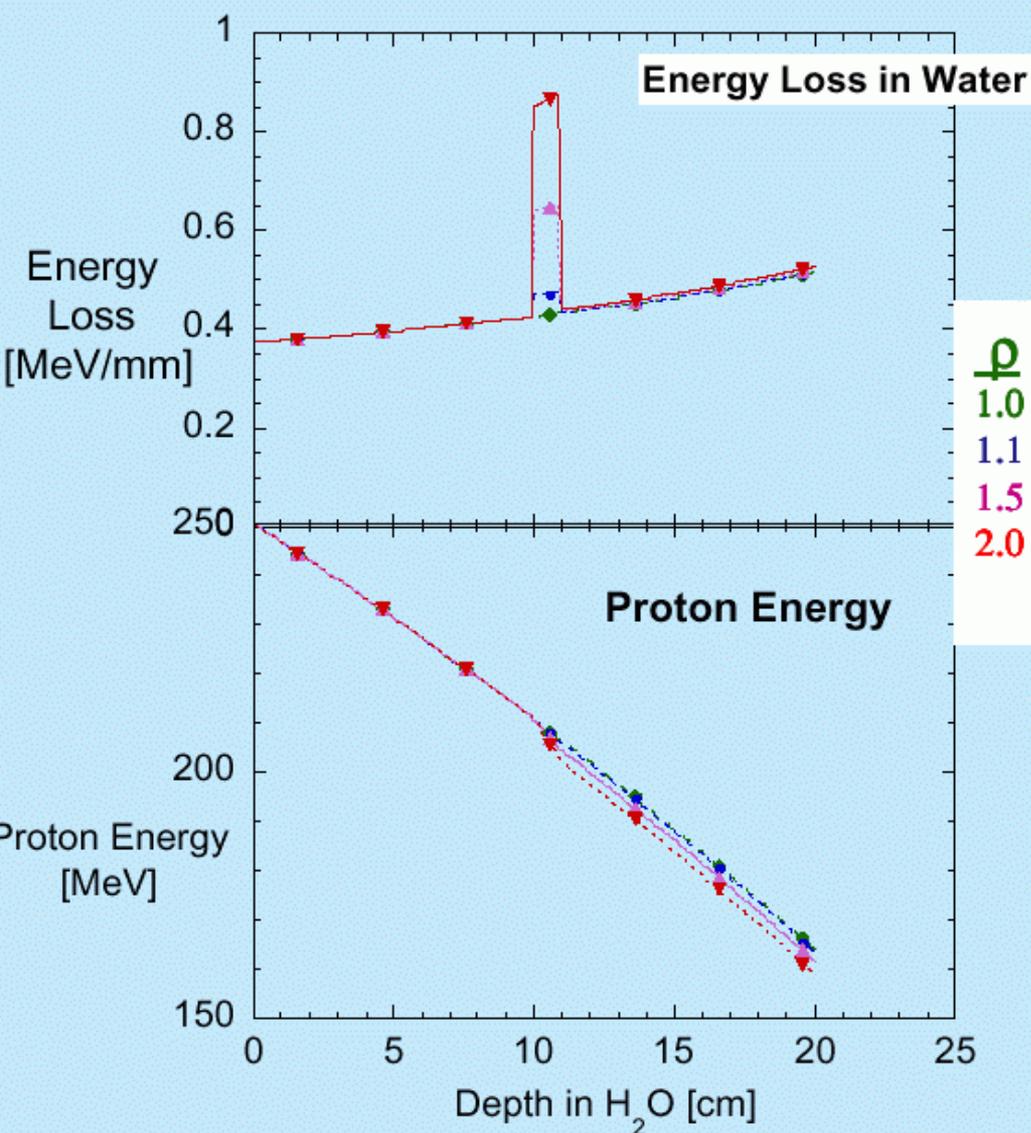
Radiograph of a phantom  
Uwe Schneider PhD thesis (PSI)



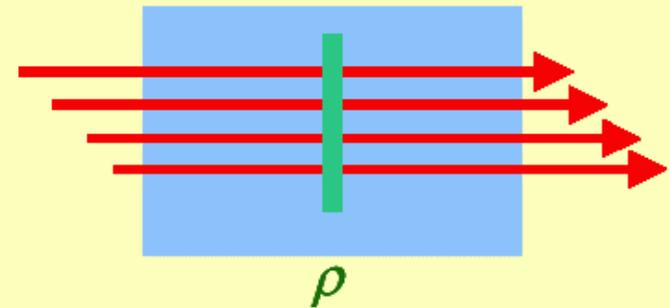
The PSI therapy gantry, with **prototype detector** in place, based on **scintillating fiber technology** (U. Schneider et al)



# Low Contrast in Proton CT

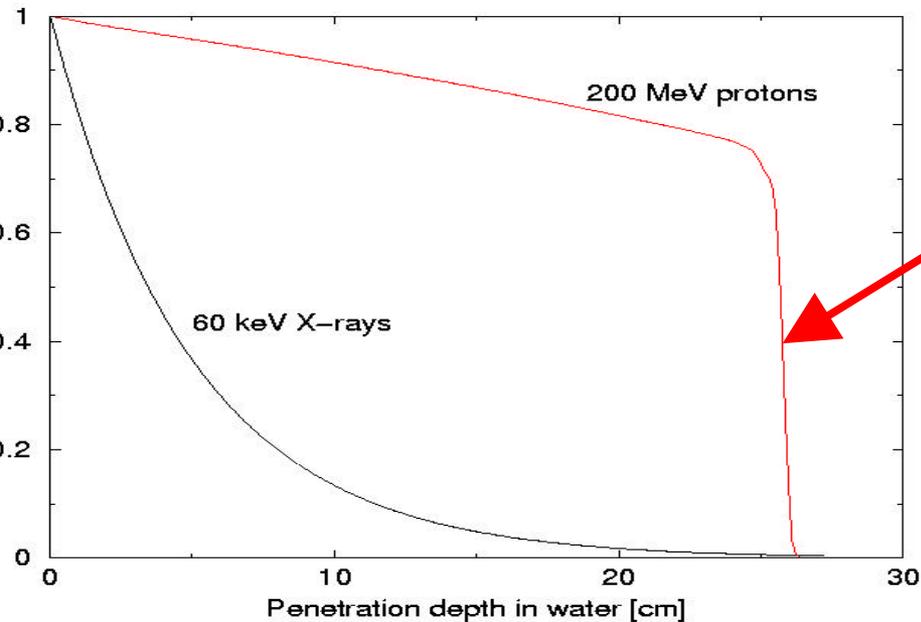


Inclusion of 1cm depth  
at midpoint of 20cm H<sub>2</sub>O



$\rho$ [g/cm <sup>2</sup> ]	Energy [MeV]	Range [cm]	TOF [ps]
1.0	164.1	38.2	1309
1.1	163.6	38.1	1311
1.5	161.5	37.7	1317
2.0	158.9	37.2	1325

# Modern techniques appear to promise ultra-low dose CT :



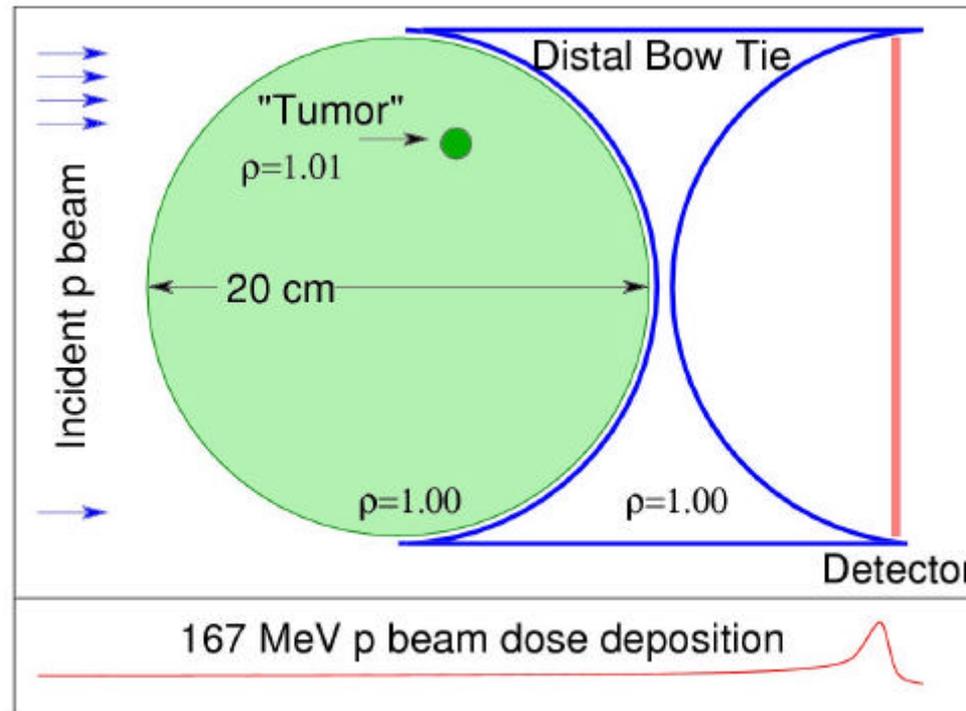
The very steep slope of transmission vs depth allows high sensitivity with few protons ...

... at especially low dose since the Bragg peak is outside the patient

Energy flexibility is desirable ...

... but is mitigated by the use of a "distal bow tie"

(Satogata et al)

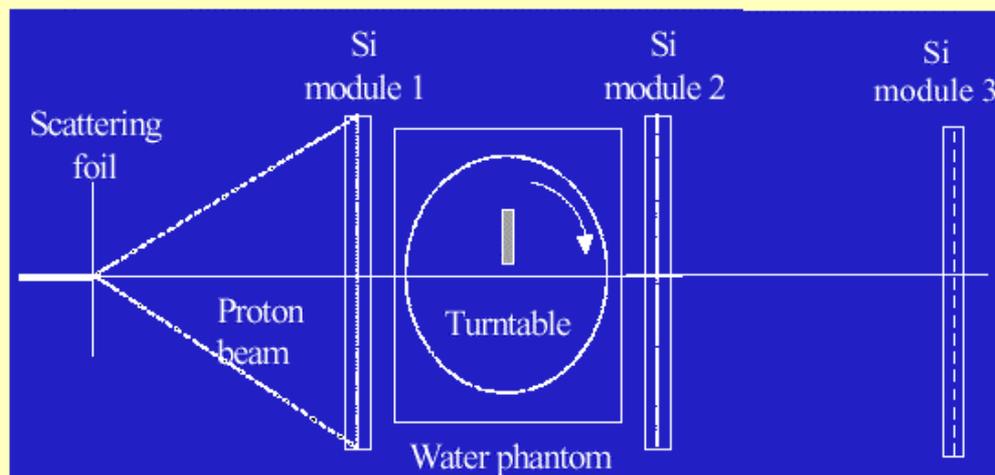


# Development of Proton Beam Computed Tomography

## Collaboration

Loma Linda University Medical Center – UC Santa Cruz

- Exploratory Study in Proton Radiography
  - two x-y detector modules
  - Crude phantom in front
- Theoretical Study
  - GEANT4 MC simulation
  - influence of MCS and range straggling
  - importance of angular measurements
  - Optimization of energy
- Experimental Study in pCT
  - Three or four x-y Si planes
  - water phantom on turntable



# Proton Energy Measurement with LET in Si

**Simple 2D Silicon Strip Detector Telescope built  
for Nanodosimetry (based on GLAST Design)**

**2 single-sided SSD**

**194 $\mu$ m Pitch**

**400 $\mu$ m thick**

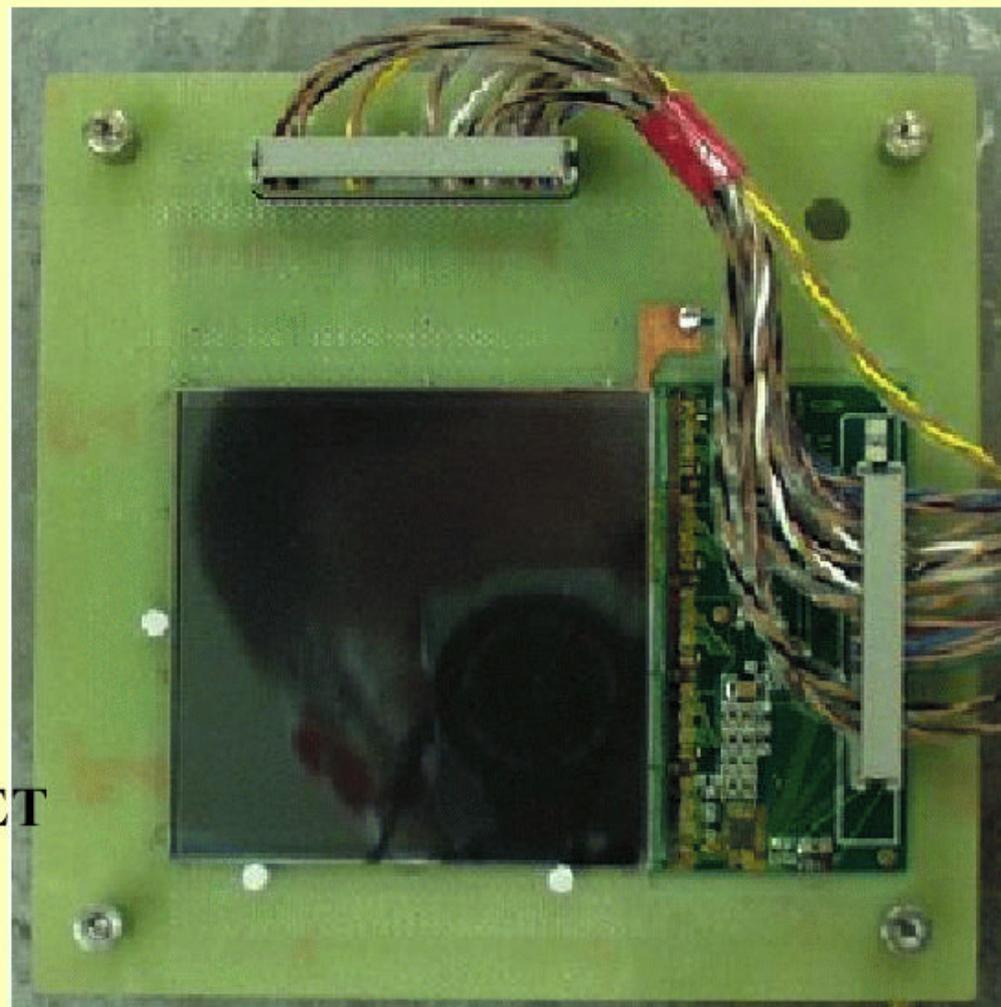
**1.3 $\mu$ s shaping time**

**Binary readout**

**Time-over-Threshold TOT**

**Large dynamic range**

**Measure particle energy via LET**



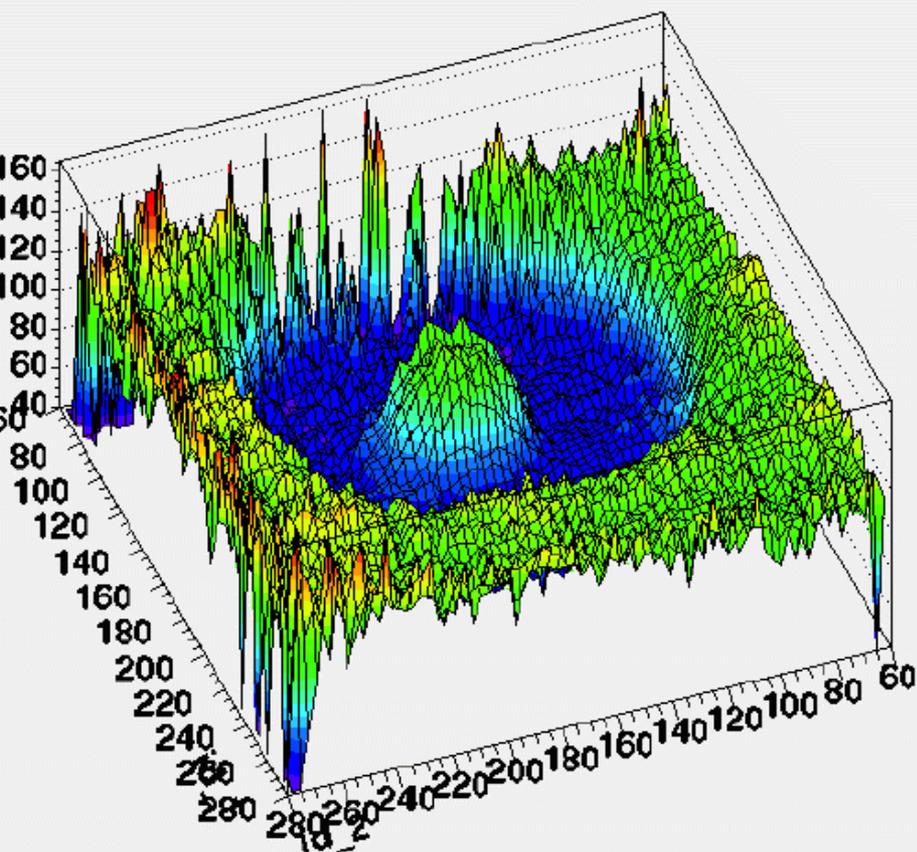
# Image !

Subdivide SSD area into pixels

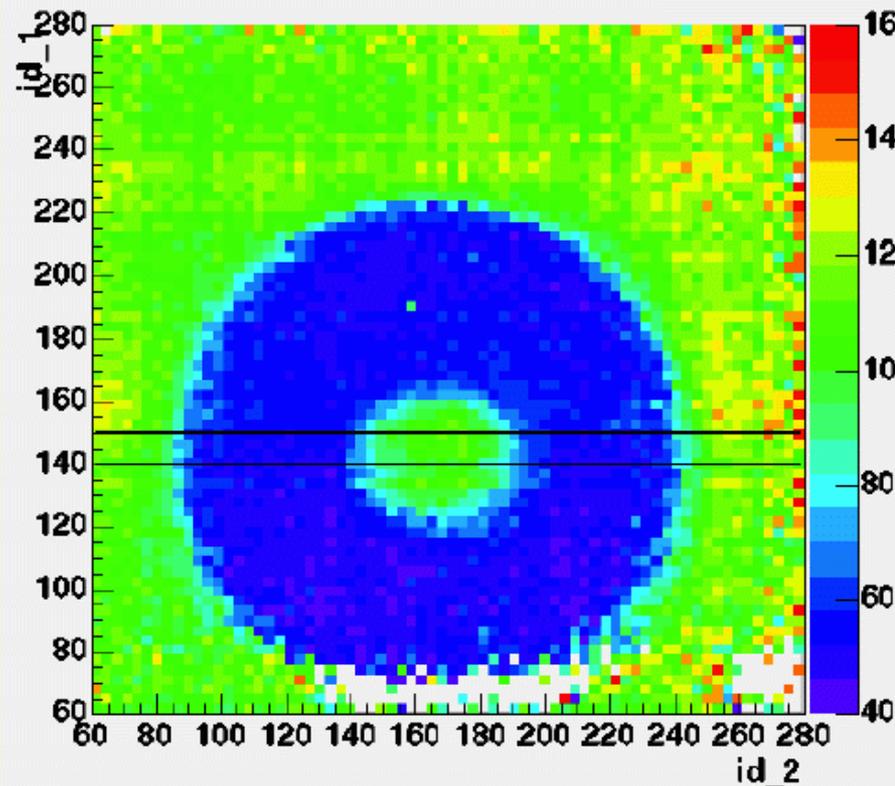
1. Strip x strip 194um x 194um
2. 4 x 4 strips (0.8mm x 0.8mm)

Image is average energy in pixel

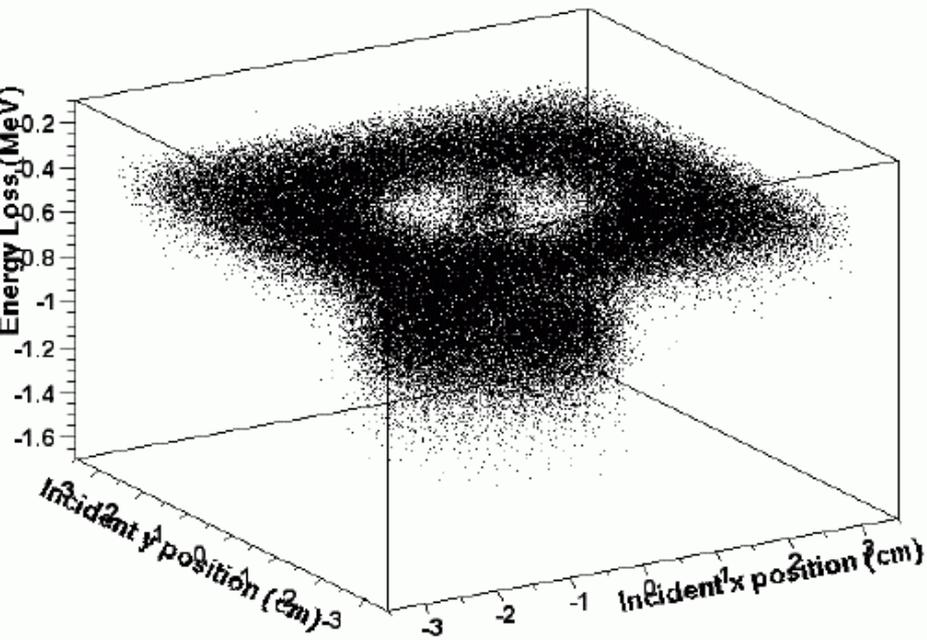
Proton Image of Al Annulus



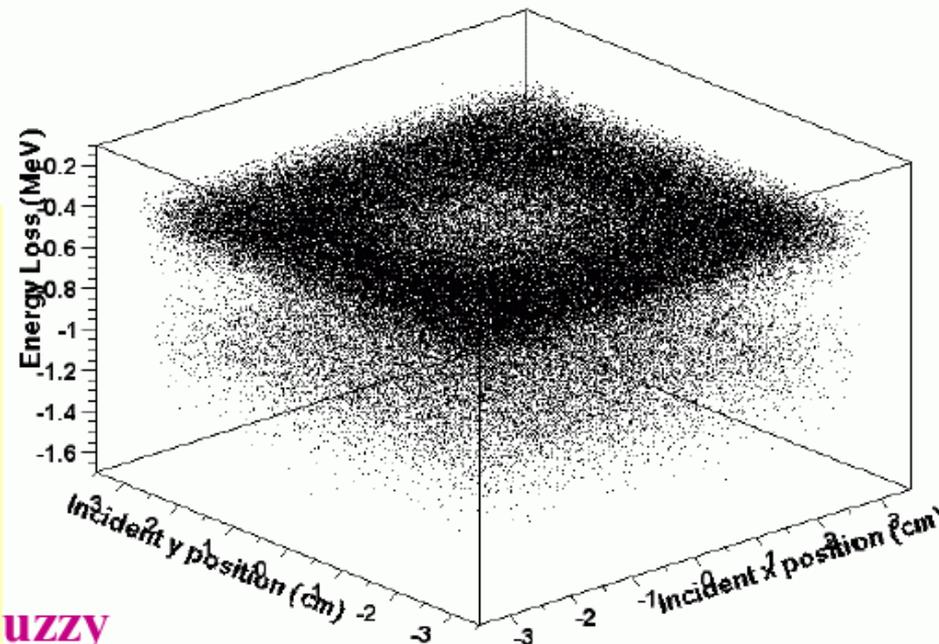
Proton Image of Al Annulus



# MC: Loss of Resolution in Back

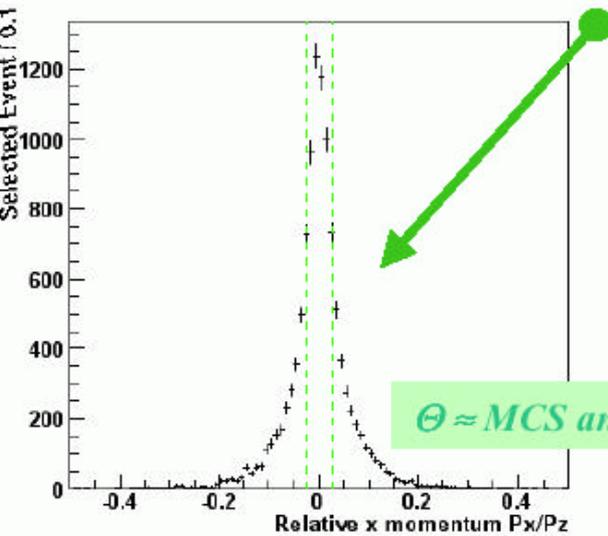


**First Plane, 2cm behind Object**



**Second Plane, 30cm behind Object: Fuzzy**

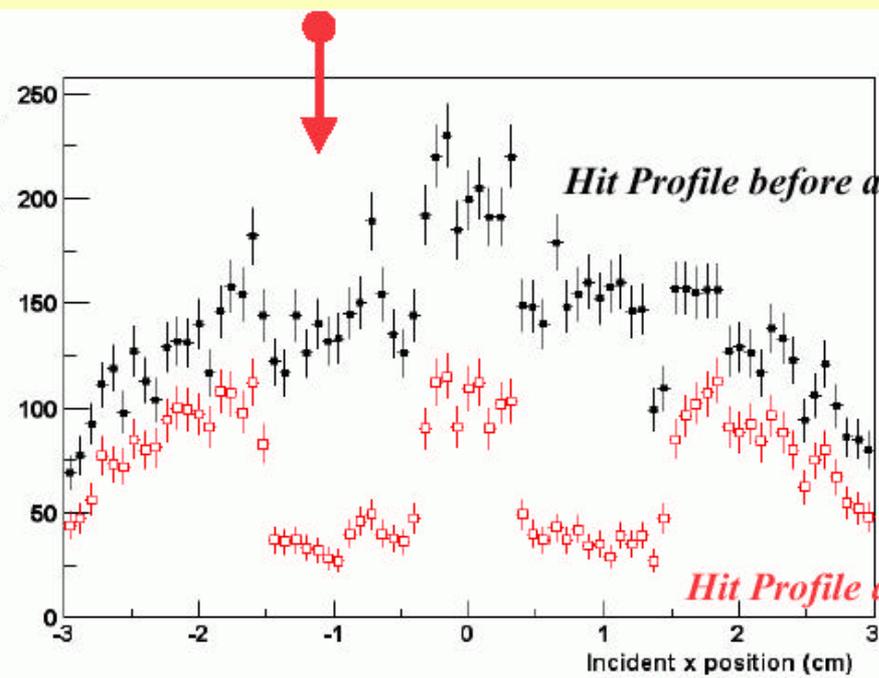
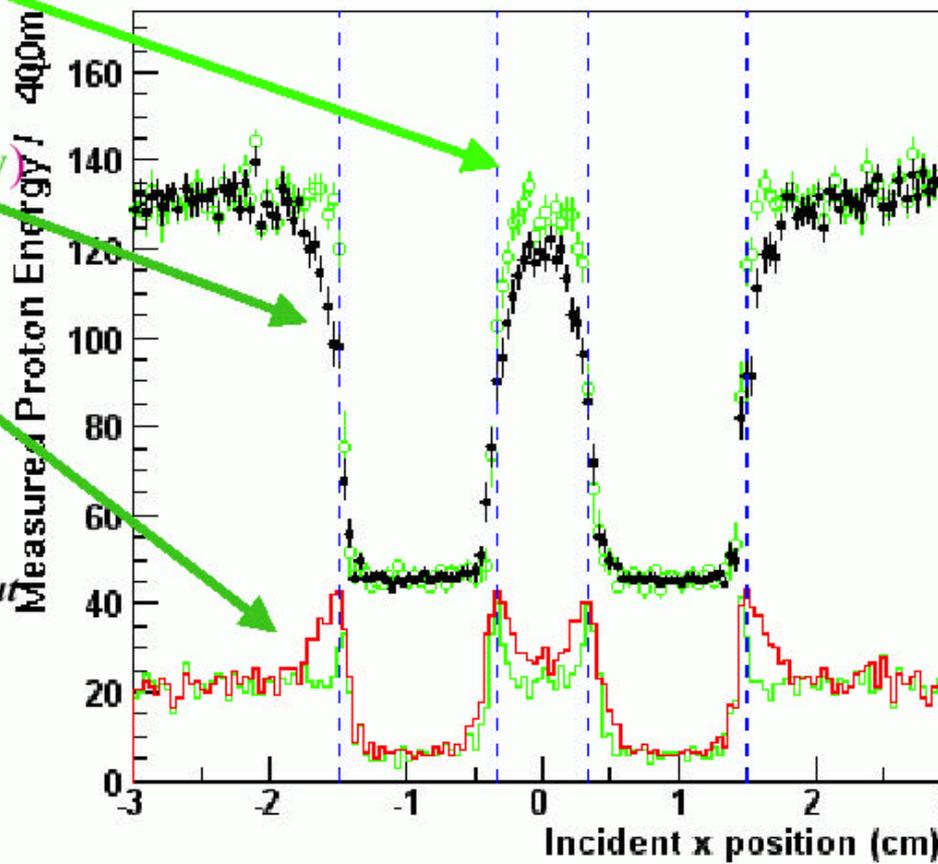
# MC: Use Angular Information



Effect of Angular Cut: Energy more uniform

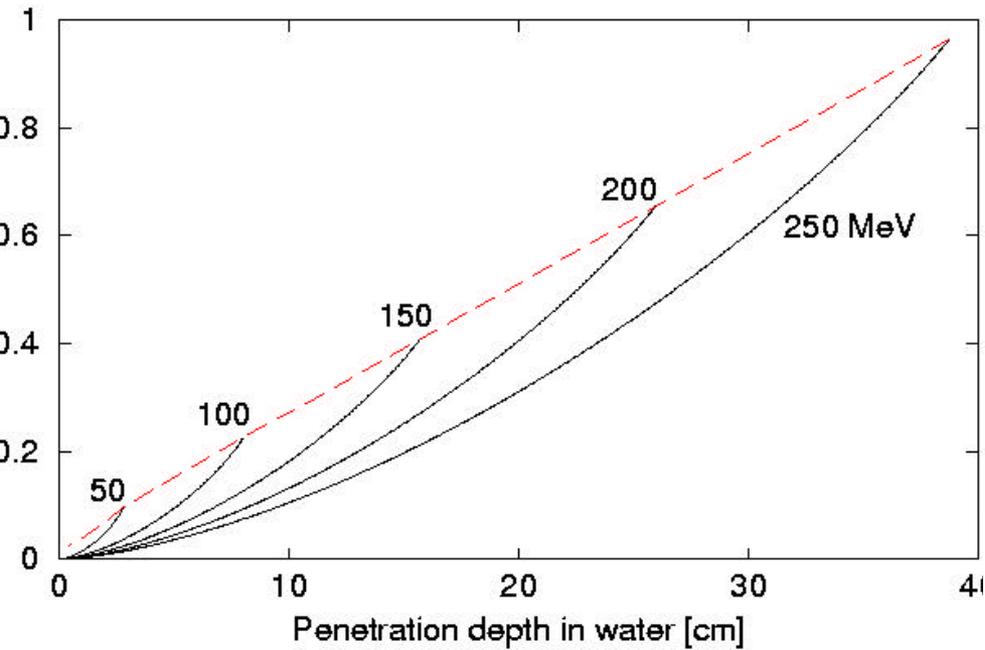
Less Migration

Sharp edges  
(RMS and Energy)



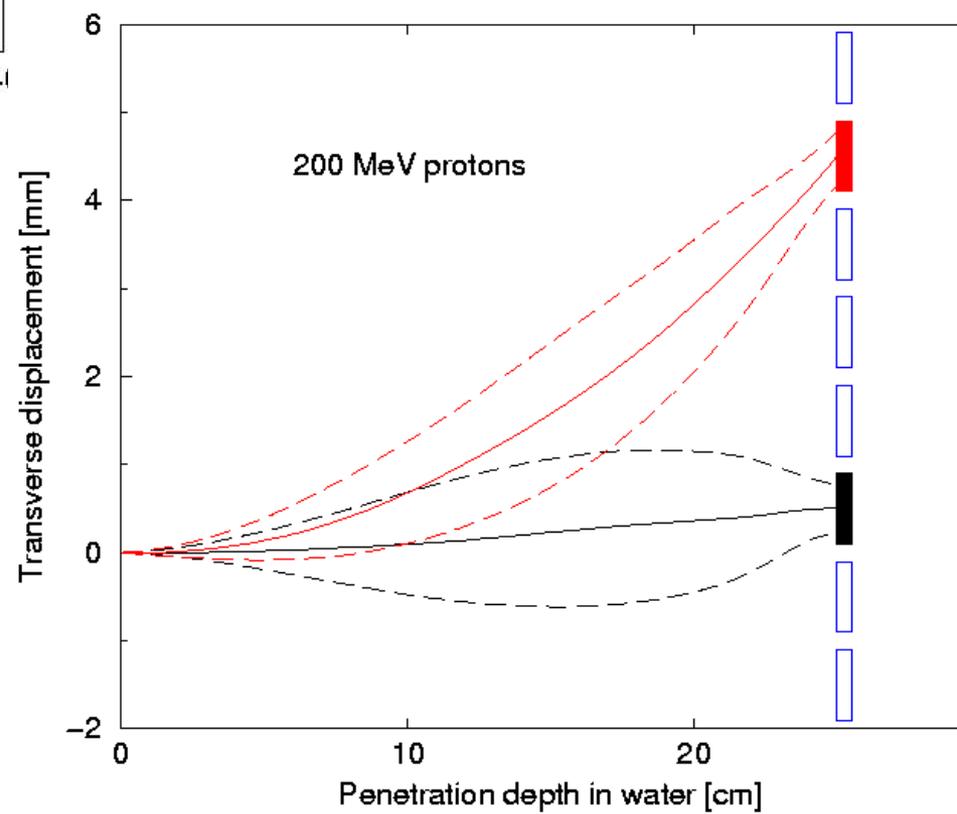
Imaging with MCS Angle?

# Multiple scattering!



Historically, proton radiography was rejected because multiple scattering made **blurry images**

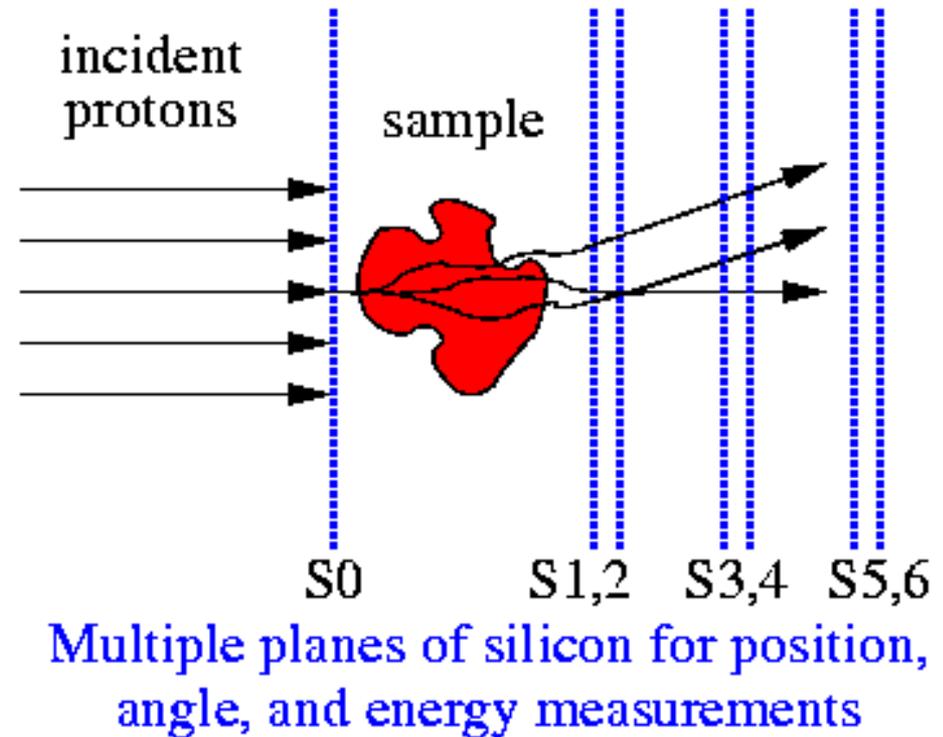
Modern reconstruction algorithms can make **sharp images** ...  
... with knowledge of **incoming and outgoing displacements and angles**



# What should a pCT imager (on a gantry) look like -- technology choice(s) ???

- scintillating fiber?
- Silicon strips?
- GEM?
- good energy resolution?

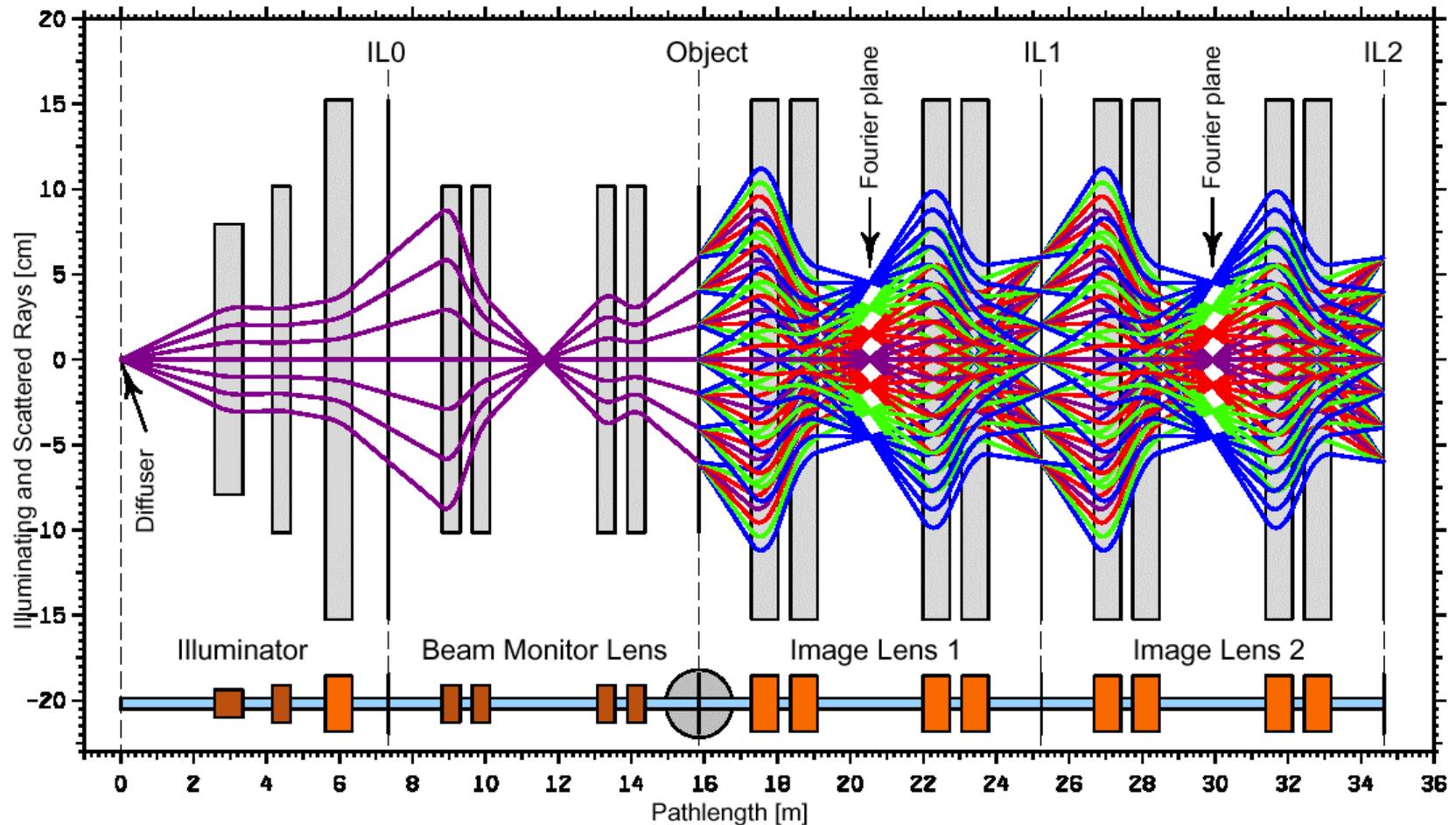
## Proton imaging spectrometer



**Transient devices: PRAD movies**

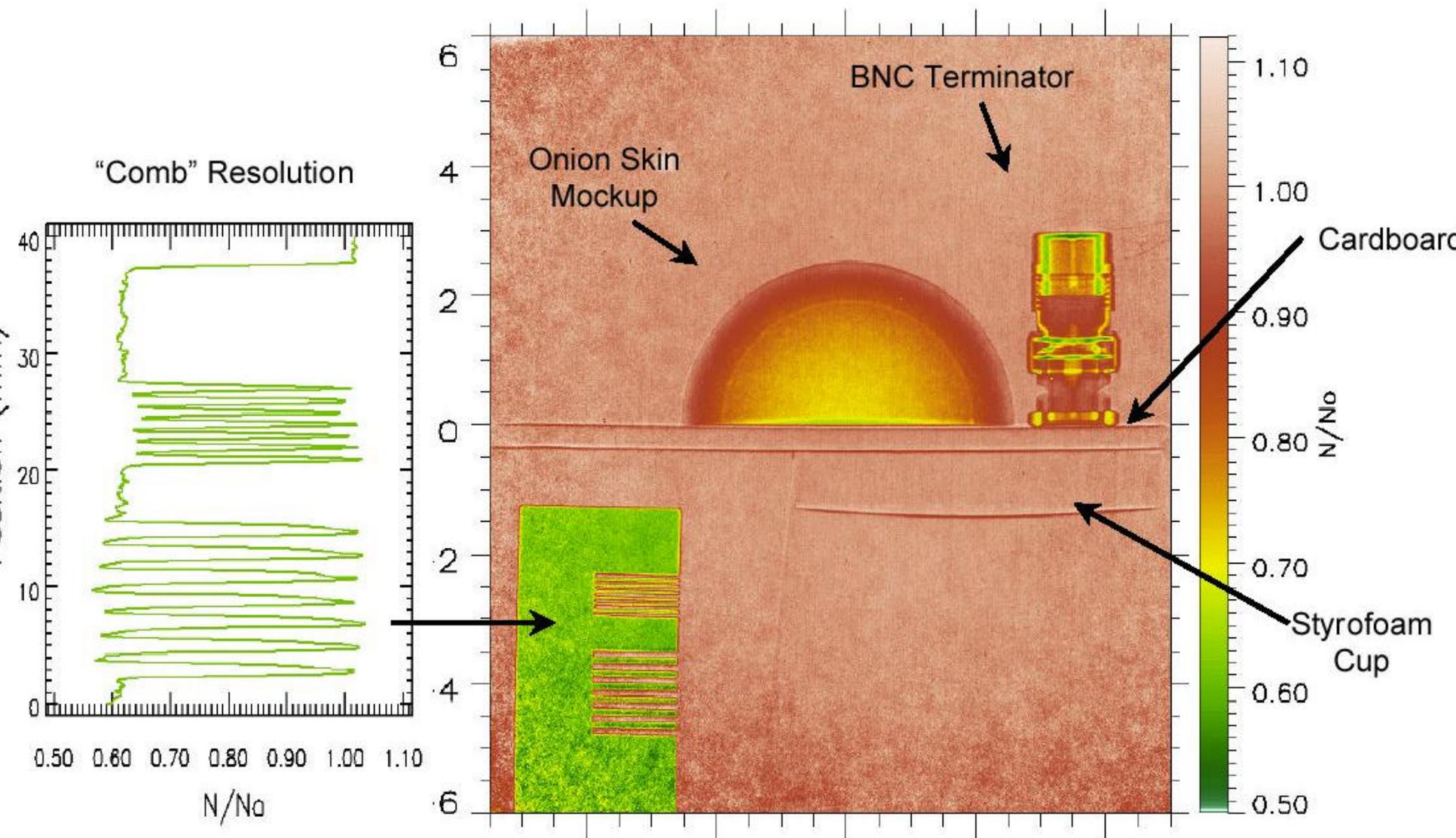
# Los Alamos beam-lines at LANSCE & BNL

Add magnetic lenses - but not on a gantry (4 GeV to 24 GeV!)



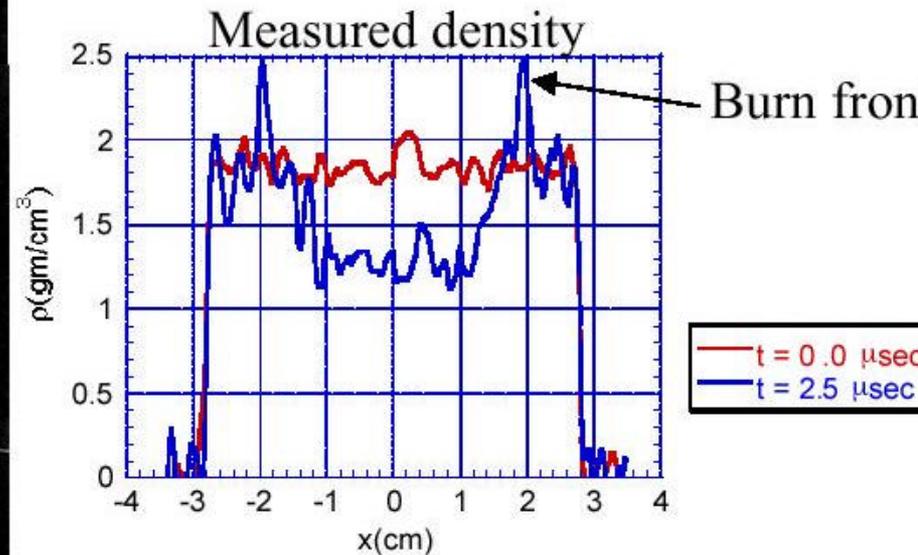
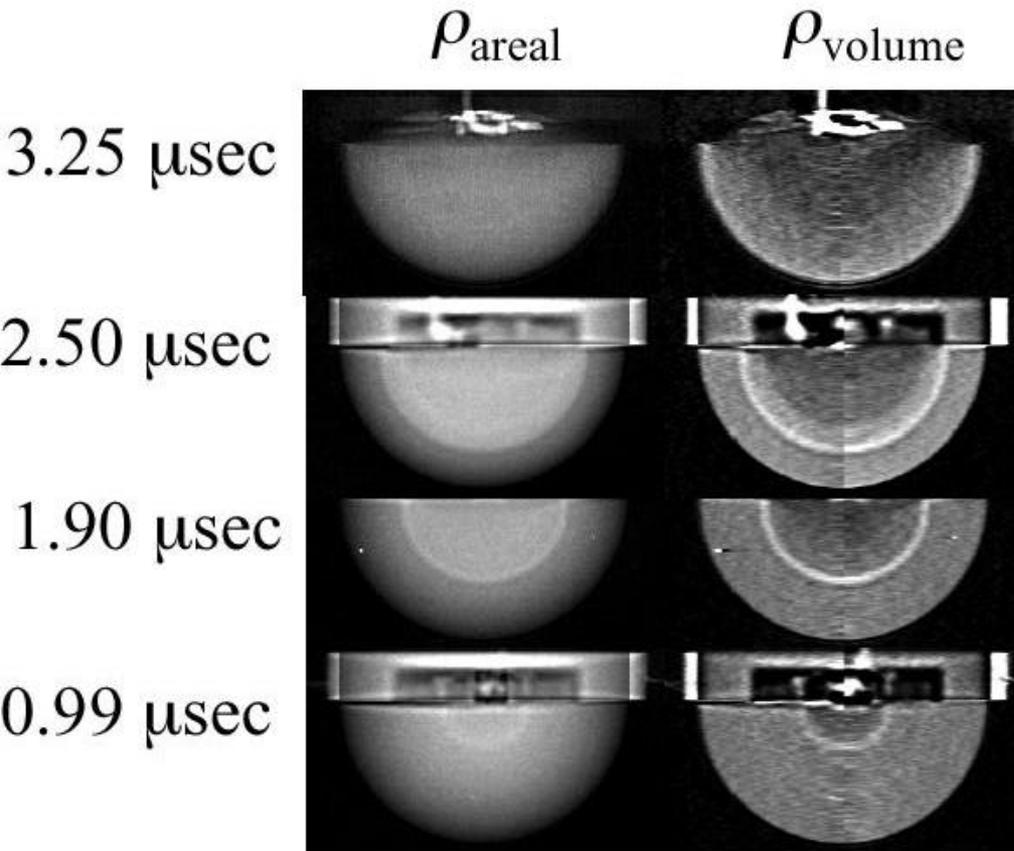
Double cuts on multiple scattering angles (at Fourier planes) enable crude material ID!

# Proton radiograph with a multi-GeV beam (Los Alamos)

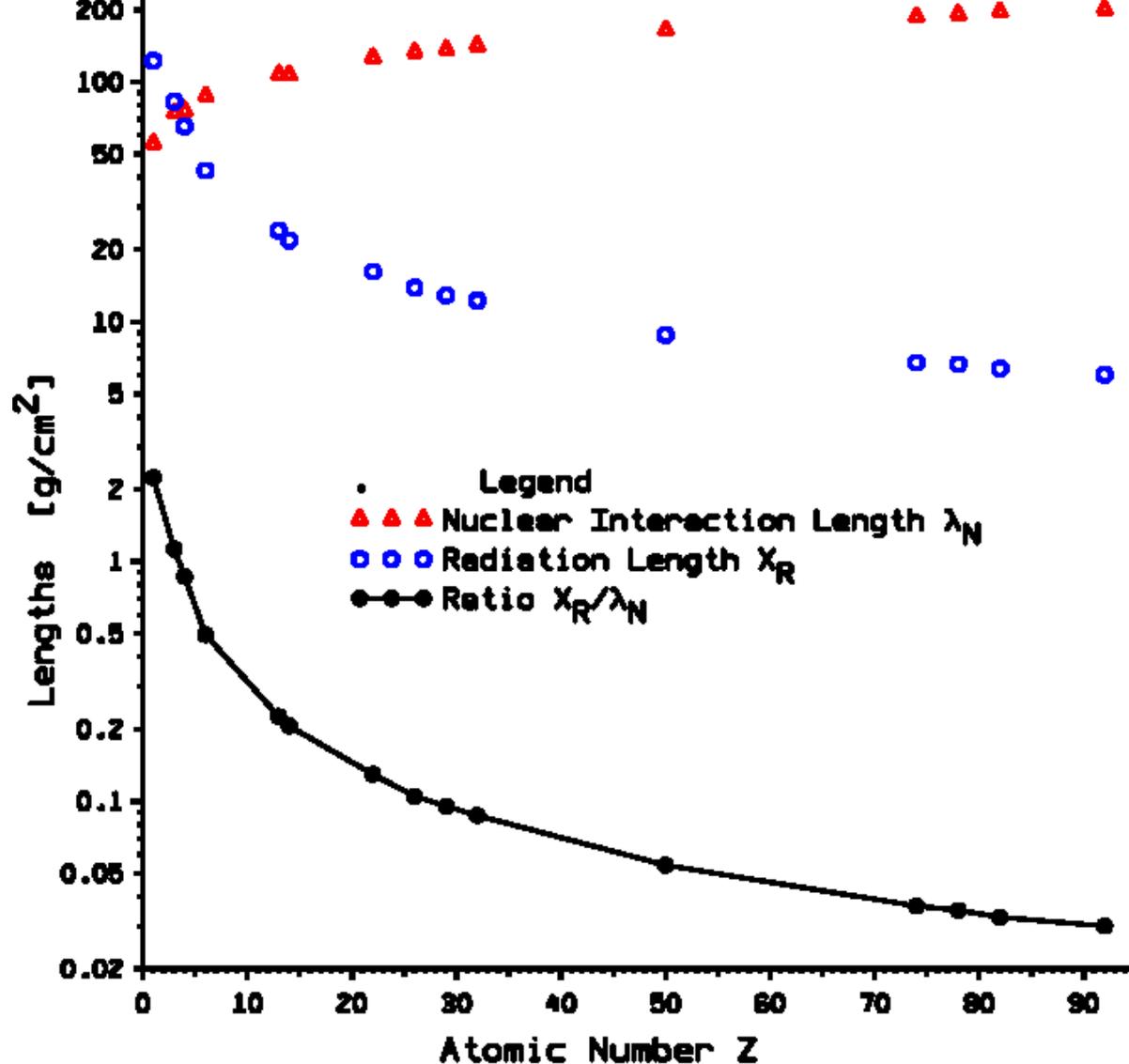


**Sub-millimeter resolution**

# Stills from a movie of a mock "device" exploding (Los Alamos)



Can also see combustion fronts inside gasoline engines, ramjets, ...



The dependence of nuclear interaction length on Z also enables crude material ID in **transmission measurements**

**Periodic CT = pCT + PRAD ??**

**The PRAD folk are exploring "civilian, periodic" systems:**

- gasoline engines**
- jet engines**

**This is a new regime that appears to benefit greatly from a hybrid approach**

- higher energies than medical**
- with magnetic lenses & spectrometers**
- with proton-by-proton tracking**

## **PRAD features, in the past:**

- fast extracted beams
- transient movies (few frames, microsecond time scale)
- transmission (intensity) measurements
- for material identification, play off
  - 1) nuclear interaction lengths
  - 2) multiple scattering
  - 3) Fourier plane imaging/collimation

## **Periodic high energy CT movies:**

- "slow" periodic systems (10,000 rpm?)
- slow extracted beam (NOT U-line, not BAF?)
- benefits from proton-by-proton tracking:
  - 1) virtual collimators (better MCS material ID)
  - 2) energy measurements (easier than medical!)
  - 3) many more (**unique!**) CT movie frames
  - 4) same modeling/algorithms as medical pCT

**Watch this space -- any comments?**

# Summary

- 1) **First generation** proton therapy facilities are "**proven**" technology. **Second generation** therapy accelerators are **arriving in force**.
- 2) For a few dollars more, put **proton imaging** on a gantry
  - a) **proton driven PET**: **high therapy dose QA**
  - b) **proton CT**: **low dose CT, treatment planning**
- 3) What does the optimal "**proton Computed Tomography**" detector look like? **Silicon? GEM? Scintillation fibers?**
- 4) **How to measure proton energies accurately?**
- 5) There appears to be an exciting field in "**CT movies**" for periodic mechanical systems, by **hybridizing pCT and PRAD** technologies!